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MECHANISM OF INTERACTION OF PEPTIDE MODIFIED NANOPARTICLES
WITH *PORPHYROMONAS GINGIVALIS*

By

Ankita Jain
B.D.S, Himachal Pradesh University, 2009

A Thesis Submitted to the Faculty of the School of Dentistry of the University of
Louisville in Full Fulfilment of the Requirements for the Degree of

Master of Science
In Oral Biology

Department of Oral Immunology and Infectious Diseases
School of Dentistry
University of Louisville
Louisville, KY

December 2016

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By

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Thesis Approved on

November 30, 2016

By the following Thesis Committee:

Dr. Donald R. Demuth. Ph. D.
Thesis Director

Dr. Jill M. Steinbach-Rankins, Ph.D.
Committee Member

Dr. Kenneth E. Palmer, Ph.D.
Committee Member

Dr. David A. Scott, Ph. D.
Committee Member

DEDICATION

To my husband Akash Ajmera

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The completion of this project could not have been possible without the participation and assistance of a lot of people whose names may not all be enumerated. Their contributions are sincerely appreciated and gratefully acknowledged.

Foremost, I want to thank The Great Almighty, the author of knowledge and wisdom, for his countless love.

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ABSTRACT

MECHANISM OF INTERACTION OF PEPTIDE MODIFIED NANOPARTICLES WITH *PORPHYROMONAS GINGIVALIS*

Ankita Jain

November 30, 2016

Studies suggest that *P. gingivalis* functions as a keystone pathogen and interacts with primary colonizers in the supragingival biofilm such as *S. gordonii*. This interaction contributes to the initial colonization of the oral cavity by *P. gingivalis* and thus represents a potential target for therapeutic intervention. We have identified a peptide (BAR) derived from the streptococcal SspB protein that functions to inhibit *P. gingivalis* adherence to *S. gordonii*. In addition, we showed that nanoparticles (NPs) functionalized with BAR inhibit this interaction more potently than free soluble peptide, possibly by promoting interaction with *P. gingivalis* at higher valency than free peptide and increasing the avidity of the interaction. Two approaches were used to assess the valency of BAR- *P. gingivalis* interaction. First NPs were conjugated with various defined amounts of BAR. The resulting NPs were tested for inhibition of *P. gingivalis* adherence using a two-species biofilm model and the results were compared with inhibition by free peptide. Nanoparticle preparations were synthesized in the presence of

increasing amounts of fluorescently labeled or unlabeled BAR. We found that peptide bound to nanoparticles increased in a dose dependent manner ranging from 1.20 μg BAR/mg of NPs to 5.87 μg BAR/mg of NPs. We tested them for inhibition in the biofilm assay. We observed dose-dependent efficacy based on the amount of BAR peptide on the nanoparticle surface. Valency of BAR peptide directly correlated to increased inhibition. Second, inhibition of adherence was also determined using BAR-antibody fusion proteins in dimer and tetramer form. Peptide-antibody fusions were produced using a plant based production platform and tested as above. We designed nucleic acid constructs that encoded BAR-antibody fusion proteins containing two or four molar equivalents of BAR. The fusion protein containing two equivalents of BAR was successfully expressed whereas the protein containing 4 BAR equivalents appeared to be toxic to cells expressing the protein. The fusion protein containing two BAR molecules showed a dose-dependent increase in the percent inhibition as the amount of the BAR peptide increased. However, the Ab-BAR fusion peptide was not more potent than soluble BAR peptide. Increasing the valency of the BAR-*P. gingivalis* interaction may pave the way for development of more potent therapeutics that target the initial colonization of the oral cavity by *P. gingivalis*.

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CHAPTER 1

INTRODUCTION

Periodontitis is one of the most ubiquitous diseases and is characterized by the destruction of connective tissue and dental bone support following an inflammatory host response secondary to infection by periodontal bacteria (AlJehani, 2014). It is the most common disease of the oral cavity, affecting soft and hard structures that support the teeth, and has many clinical outcomes including loss of attachment, bone loss and eventually tooth loss (Albandar, 2011; Dhadse et al, 2010). Periodontitis is second only to dental caries as a cause of tooth loss among adults in developed countries (Gautam et al., 2011). A study entitled *Prevalence of Periodontitis in Adults in the United States: 2009 and 2010* estimates that 47.2 percent of the American adults or 64.7 million Americans have mild, moderate or severe periodontitis (Eke et al., 2015). In adults, 65 years and older, the prevalence rate increases to 70.1 percent (Eke et al., 2015). Other studies have demonstrated that mild forms of periodontitis affect 75% of adults in the United States and more severe forms affect 20 to 30% of adults (Dhadse, et al, 2010). A study conducted combined the data from the

2009 to 2010 and 2011 to 2012 cycles of the National Health and Nutrition Examination Survey (NHANES). It concluded high prevalence of periodontitis in US adults aged ≥ 30 years, with almost fifty-percent affected (Eke et al., 2015). In the early stage of periodontitis, termed gingivitis, gums become swollen and red due to inflammation, which is the body's natural response to the presence of harmful bacteria. The colonization of bacteria in the supragingival area initiates an inflammatory response which leads to periodontitis (Brogden & Guthmiller, 2002; Dickinson et al., 2011). Currently, treatments like removal of dental plaque, antibiotic therapy or gingival surgery (if required) may help to cure periodontitis. No therapeutic method has been devised to actually prevent the colonization of bacteria, thereby, preventing biofilm formation.

Biofilm

A biofilm is a structured community of micro-organisms that is adhered to a surface and enclosed in a self-generated matrix (consisting of carbohydrate polymers, proteins, and DNA) (Donlan, 2002). Microbial biofilms are known to cause a number of infectious diseases in humans, a few of which include tonsillitis, dental disease, urinary tract infections and endocarditis (Bjarnsholt, 2013). Dental plaque is a complex oral multispecies biofilm that adheres to the teeth and consists of many species of both fungal and bacterial cells. According to World Health Organization, it is a specific but highly variable structural entity resulting from sequential colonization and growth of microorganisms on the surfaces of teeth and/or restorations (Rosan & Lamont,

2000). The biofilm consists of microorganisms of various species embedded in an extracellular matrix composed of bacterial metabolic products and substances from serum, saliva and blood. This accumulation of microorganisms subjects the teeth and gingival tissues to high concentrations of bacterial metabolites, often resulting in gingivitis and eventually periodontitis. Therefore, understanding the development of dental plaque and the corresponding etiology of periodontitis would help to develop therapeutics to prevent or cure periodontitis.

Development of Dental Plaque

The formation of biofilms occurs in a multistep progression (O'Toole et al, 2000). Obtaining a better understanding of the mechanisms of bacterial attachment and co-adhesion could lead to strategies to control or influence the pattern of biofilm formation. Distinct stages in plaque formation include the following stages depicted in Figure 1 (Chandki et al, 2011; Dickinson et al., 2011; Marsh, 2006)

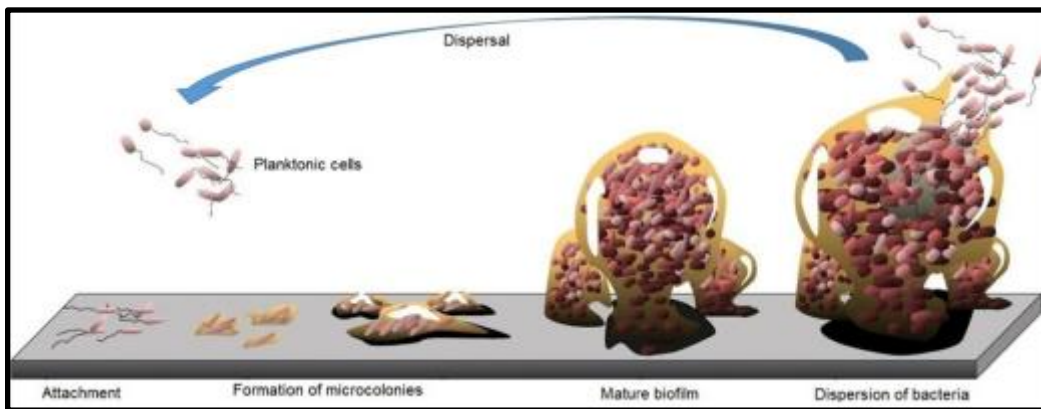


Figure 1: Stages in biofilm formation. * adapted from wikipedia.org/wiki/File:Biofilm.jpg

Plaque formation begins with the formation of the acquired pellicle (Diaz et al., 2006). The pellicle is a thin coating of salivary proteins that adheres to the tooth

surface within minutes after tooth eruption or cleaning (Armstrong, 1968). The pellicle is composed of albumin, glycoproteins, acidic proline-rich proteins, mucins, cell debris, amylase, lysozyme and sialic acid (Lindh et al, 2014). The pellicle provides a sticky base to support further microbial colonization (Lindh et al., 2014). Acidic phosphoproteins and proline-rich proteins mediate initial interactions with primary colonizing organisms, which are comprised largely of Gram-positive cocci, including streptococcal species (Marsh, 1994; Marsh, 2006).

After pellicle formation, reversible adhesion contributes to the beginning of bacterial cell attachment (Garrett et al, 2008). Reversible adhesion involves weak long-range physicochemical interactions between the cell surface and the pellicle, which can lead to stronger adhesin-receptor mediated attachment (Garrett et al., 2008). Reversible adhesion is initiated with a single cell adhering to the surface from a 'planktonic' state, in which the bacteria are freely floating in the solution that bathes the oral cavity (Garrett et al., 2008). This change from the 'planktonic' state is usually associated with the change in the expression of genes and also the phenotype leading to the adaptation of bacterial cell lifestyle from the planktonic environment to the environment on the tooth surface.

After reversible adhesion, the cells start to proliferate and form microcolonies.

This process may increase the diversity of the biofilm through co-adhesion between different species (Grenier, 1992; Kinder & Holt, 1989; Kolenbrander & Andersen, 1989). This results in the attachment of secondary colonizers to already adhered cells. Co-adhesion is driven by specific receptor-ligand

interactions that allow new bacterial colonizers to adhere to the previously attached cells and results in increased complexity of the microbial community (Grenier, 1992; Kinder & Holt, 1989; Kolenbrander & Andersen, 1989).

At this stage, the microcolonies begin to produce an extracellular matrix comprised of extracellular carbohydrates and genomic DNA. The microcolonies continue to proliferate and develop into 'mature biofilms' that are characterized by vertical growth on the solid surface. The mature biofilm is a complex structure comprised of towering microcolonies interspersed with fluid filled channels, which provide nutrients and oxygen that are required for normal bacterial growth. The channels are also conduits that facilitate the outward movement of bacterial metabolites, waste products, and enzymes.

This biofilm life cycle is completed by the release of the bacterial cells back into the 'planktonic' state either by an 'active' or 'passive' process, known as detachment. In the active process, the cell itself may produce enzymes that cleave the matrix, reducing the integrity of the matrix and facilitating the release of cells. Alternatively, cells in the biofilm may stop production of enzymes that produce the matrix. Thus the biofilm may become exposed and disintegrates. In addition, 'passive' processes may also lead to the release of bacterial cells into a free floating state, which can then recolonize a new surface. For example, the physical abrasion of the tongue against the tooth may facilitate biofilm removal. During the process of biofilm formation, quorum sensing and other signal transduction pathways play an important role in biofilm growth and maturation. For example, the process by which bacterial cells adhere and interact with a

surface can initiate new genetic programs, allowing the microorganism to survive in the new environment (Blango & Mulvey, 2009). This is called 'contact-dependent signaling'. Contact dependent signaling can also occur between two different organisms. This interspecies adherence can stimulate new genetic programs that allow cells to alter their genetic profiles to enhance viability in the microbial community (Blango & Mulvey, 2009).

Significance of Etiology of Periodontitis

Some of the bacteria that contribute to the oral microbiotic community include *Porphyromonas gingivalis*, *Tannerella forsythia*, and *Treponema denticola* (Suzuki et al, 2013). These species are considered 'periodontopathogens', and are classified as 'red' complex oral bacteria that have a strong association with each other and with diseased sites in chronic adult periodontitis (Darveau et al, 2012; Suzuki et al., 2013). Two main hypotheses may explain the role of plaque bacteria in a diseased individual. The "Specific Plaque Hypothesis" asserts that only specific species are involved in causation of disease, even if present in low abundance (Hajishengallis, 2014; Hajishengallis & Lamont, 2012; Loesche, 1992; Rosier et al, 2014). One of the 'red complex' bacteria, *P. gingivalis*, has been described to function as a keystone pathogen (Hajishengallis & Lamont, 2012; Rocas et al., 2001; Rosier et al., 2014). It disrupts host-microbe homeostasis in the oral cavity leading to dysbiosis even in low abundance, and is thus strongly associated with adult periodontitis (Hajishengallis & Lamont, 2012). Given this impact at low abundance, it is believed that *P. gingivalis* alters the host response

and induces changes in microbial biofilm populations, prompting uncontrolled inflammation and tissue damage (Darveau, 2010; Hajishengallis & Lamont, 2012; Loesche, 1992). However, this hypothesis cannot completely explain the absence of presumed pathogens in some diseased individuals or the presence of these pathogenic organisms in healthy patients (Darveau, 2010). Contrary to this, the "Non-Specific Plaque Hypothesis" proposes that periodontitis is a result of the overall interaction of the plaque microflora with the host (Hajishengallis & Lamont, 2012; Rosier et al., 2014). It is well established that plaque-mediated diseases have a multi-factorial etiology and a variety of organisms are involved in its progression (Hajishengallis & Lamont, 2012; Rosier et al., 2014). Considering both theories, a modified hypothesis has been proposed suggesting that changes in environmental factors lead to a shift in the resident microflora resulting in microbial dysbiosis (Rosier et al., 2014). This modified hypothesis supports the occurrence of potentially pathogenic species as minor members of the resident plaque microflora (Rosier et al., 2014). Certain low-abundance microbial pathogens can cause inflammatory disease by interfering with the host immune system and remodeling the microbiota (Hajishengallis & Lamont, 2012; Rosier et al., 2014). In healthy individuals, these organisms would be weakly competitive and significantly suppressed by intermicrobial antagonism (Hajishengallis & Lamont, 2012; Rosier et al., 2014). As such, they would comprise only a small percentage of the plaque microflora and would have limited clinical significance (Rosier et al., 2014).

P. gingivalis and its interaction pattern

Apart from being considered a keystone pathogen, *P. gingivalis* has long been associated with periodontitis, has a well-characterized population structure, and demonstrates the “easiest” growth and genetic manipulation of the three ‘red complex’ bacteria (Rocas et al., 2001). Due to these factors, *P. gingivalis* has garnered much attention and has been well-studied (Curtis et al., 2011; Darveau et al., 2012; Lamont & Jenkinson, 1998). *P. gingivalis* is a pathogen whose primary niche is in the anaerobic environment of subgingival dental plaque; however, initial colonization occurs on supragingival surfaces that already support robust biofilm communities in oral cavity (Daep et al., 2006). Studies suggest that biofilm formation occurs subsequent to initial adherence of *P. gingivalis* to *S. gordonii* cells deposited on the salivary pellicle (Cook et al., 1998). The interaction between *P. gingivalis* and *S. gordonii* is one of the many critical interactions which promote biofilm formation. Targeting this particular interaction may inhibit the biofilm formation more effectively, if not completely. The commensal species *S. gordonii* provide an attachment substrate for colonization and biofilm accretion by the potential pathogen, *P. gingivalis* (Cook et al., 1998). Due to this favorable interaction, *P. gingivalis*, has been shown to specifically adhere to primary colonizing bacteria such as *S. gordonii* (Park et al., 2005). Considering this, the initial colonizing mechanism of *P. gingivalis* is a primary target to inhibit biofilm formation with rationally designed therapeutics that prevent initial supragingival colonization (Daep et al., 2006).

BAR Peptide

P. gingivalis is a leading pathogen implicated in chronic adult periodontitis (Kozziel et al., 2014). Previous studies have shown that *P. gingivalis* adheres to *S. gordonii* through the interaction of the minor fimbrial antigen, Mfa1, with a specific region of the streptococcal SspB polypeptide which has been designated BAR (SspB Adhering Region) (Chung et al., 2000; Daep et al., 2006; Daep et al., 2008; Demuth et al., 2001; Lamont et al., 2002). It has been shown that a synthetic peptide comprising the BAR sequence potently inhibits *P. gingivalis* adherence to *S. gordonii* (IC₅₀=1.3 μM) (Daep et al., 2006; Daep et al., 2008; Daep et al., 2011). Moreover, BAR peptide significantly reduced *P. gingivalis* virulence in mice that harbor *S. gordonii* when administered simultaneously with *P. gingivalis* cells (Daep et al., 2011). However, the effects of BAR administration demonstrated transient effects, and exhibited weaker potency against pre-existing or more complex biofilms. In more complex biofilms, the IC₅₀ increased to 3.6 μM and an exposure time of more than 60 minutes was required to achieve equivalent effects as achieved in two species biofilms (Demuth, unpublished). These limitations to clinical translation spurred the need to develop novel approaches to deliver BAR peptide at higher localized concentrations to increase efficacy. Our recent studies suggested that poly (lactic-co-glycolic acid) (PLGA) nanoparticles (NPs) that are surface-functionalized with BAR inhibit *P. gingivalis* and *S. gordonii* interactions more potently than free soluble peptide (Steinbach-Rankins and Demuth, unpublished).

Advantages of Nanoparticles as advanced therapeutics

Nanoparticles are being studied extensively as a delivery method for antimicrobials for various diseases (De Jong & Borm, 2008; McMillan, Batrakova et al., 2011; Singh & Lillard, 2009). They offer many advantages over conventional therapeutic approaches that deliver free antimicrobials via oral, submucosal, or localized delivery routes (Gelperina et al., 2005; Ikuma et al., 2015; Singh & Lillard, 2009). First, due to their small size, NPs can penetrate barriers to deliver higher concentrations of active agents at target sites, providing increased efficacy (Mudshinge et al. , 2011; Singh & Lillard, 2009). Second, NPs can be tailored to recognize specific cell types simply by altering their surface-chemistry (Mudshinge et al., 2011; Singh & Lillard, 2009). Moreover, NPs allow for prolonged delivery of drugs which helps to increase the efficacy of the drugs for increased durations under often adverse physiological conditions *in vivo* (Hong et al., 2007; Puglia et al., 2008; Singh & Lillard, 2009). Also, NPs may promote multivalent binding which can act to increase the potency of active agents (Hong et al., 2007). In addition to this, NPs promote the stability of active agents *in vivo*, by protecting the agent from degradation. Apart from these advantages, NPs can carry a diversity of hydrophilic and hydrophobic active agents (e.g. drugs, proteins, peptides, genes, etc.) that can be co-incorporated in the NP matrix and can be administered orally, locally and intravenously (Mody et al., 2010; Mudshinge et al., 2011; Singh & Lillard, 2009)

Nanoparticle Types

NPs have been developed using a variety of materials including metals, ceramics and polymers (Abiodun-Solanke et al., 2014; Adeyemi & Sulaiman, 2015; De Jong & Borm, 2008; Wang & Wang, 2014). Silver NPs have been widely used in dentistry to fabricate new materials like cements or resins (Arvizo et al., 2012; Batra & Miglani; Ge et al., 2014; Batra et al. 2016). Magnetic NPs like magnetite and maghemite, which are comprised of iron oxide, have been actively studied for cancer and gene therapy applications (Gobbo et al., 2015; Herranz et al., 2011; Batra et al. 2016, unpublished). Copper, zinc, titanium dioxide and quaternary ammonia NPs have demonstrated antimicrobial activity and their hydrophobic nature and surface charge add to their antimicrobial activity (Batra et al. 2016, unpublished). Many of the metal-based NPs have imparted antimicrobial properties that have proven beneficial to oral health by improving the interaction of therapeutics with bacterial biofilms and inhibiting the biofilm formation (Allaker, 2010; Senior et al., 2012; Sirelkhatim et al., 2015; Batra et al., 2016). The proposed mechanism of these antibacterial activities is believed to arise from an electrostatic attraction of positively-charged NPs with the negative charge of the bacterial cell membrane (Palza, 2015; Singh & Lillard, 2009). Other novel systems using silica NPs and nitric oxide NPs are being studied for to prevent biofilms as well (Kafshgari et al., 2014; Batra et al. 2016). However, despite these attributes, there have been several concerns regarding the toxicity associated with the metallic NPs and their accumulation in various tissues and organs (Niazi & Gu, 2009). To avert the toxicity associated with metal

NPs, polymeric NPs have the potential to offer a safer and more biocompatible delivery method.

Polymeric NPs

Polymeric NPs have demonstrated biocompatibility and flexible tuning of physical properties enabling the drug release and dosage profiles. There are many types of polymeric NPs including poly (lactic acid) (PLA), poly(ϵ -caprolactone) (PCL), polyethyleneimine, poly (lactic-co-glycolic acid) (PLGA) and poly (glycolic acid) (PGA). These polymers have been extensively used to prevent oral biofilms due to their biodegradability and biocompatibility (Allaker, 2010; Wang et al., 2016). Furthermore, polymeric NPs comprised of PLA and PGA, have the ability to degrade into relatively inert metabolic by-products, enabling safe and non-toxic delivery of associated cargo.

PLGA Nanoparticles

PLGA NPs have been FDA-approved for use in human therapy which is one of the primary reasons for extensive research using these particles (Makadia & Siegel, 2011). PLGA can deliver hydrophilic and hydrophobic small molecules as well as larger macromolecules due to its well described formulation protocols (Martin-Banderas et al., 2013). PLGA NPs are being tested for use in photodynamic therapy, which when introduced into a bacterial cell, release singlet oxygen and free radicals to destroy bacterial cells (Li & Huh, 2014). In other work, PLGA NPs that encapsulate methylene blue have demonstrated

efficacy against Gram-positive as well as Gram-negative bacteria associated with endodontic as well as periodontal infections (Klepac-Ceraj et al., 2011). In addition to the attributes that encapsulation provides, PLGA NPs can be surface-modified to provide specific targeting and enhanced therapeutic outcomes (Makadia & Siegel, 2011). Advanced studies are still being done to impart knowledge about the basic functionality of the PLGA NPs with various peptide modifications, yet these are considered to be promising antimicrobials delivery vehicles relative to less specifically-acting conventional therapeutics (Makadia & Siegel, 2011).

Our preliminary studies have suggested that PLGA NPs that are surface-modified with BAR peptide increase the effectiveness of peptide-mediated inhibition of *P. gingivalis*-*S. gordonii* adherence. A possible mechanism by which these NPs enhance the potency is by promoting a multivalent binding interface to increase the avidity of BAR with *P. gingivalis*, or by delivering BAR at a higher localized concentration to *P. gingivalis*. In fact, many studies have demonstrated that multivalent interactions are more efficacious in increasing the avidity of peptides relative to monovalent interactions (Figure 2) (Wang et al., 2016). In one study, a specific special multivalent effect was observed for polymeric NPs displaying galactan, resulting in a significant increase in binding, relative to free glycan (Bonduelle et al., 2016). In another study, multivalent targeting approach was shown to have the potential to amplify AT1R (Angiotensin 1 Receptor) blockade in the eye and concomitantly deliver a therapeutic payload into ocular lesions choroidal vasculature (Hennig et al., 2015). Similar to these studies, we

expect that the increase in potency of the surface modified NPs may be due to the increase in the valency.

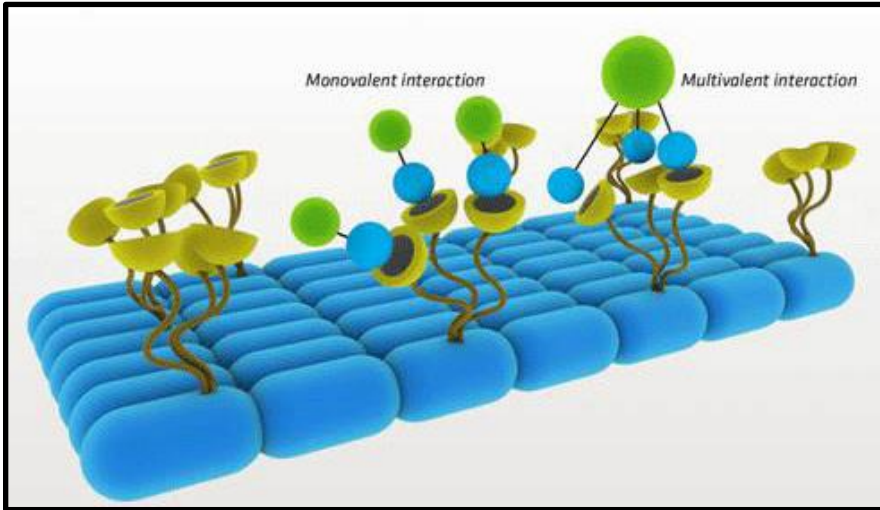


Figure 2 Comparison of monovalent and multivalent interactions. Multivalent interactions are considerably stronger than the individual bonding of a corresponding number of monovalent ligands to a multivalent receptor and are often used in biological systems. Adapted from Prof. Dr. Rainer Haag research topics.

Drug delivery by binding to Immunoglobulins

Therapeutic drugs and proteins often suffer from short half-life; mainly due to their small size or rapid clearance by enzymes. Genetic modification of these drugs or proteins employing various techniques can improve the pharmacokinetics by prolonging the half-life by either preventing excretion or degradation in the body. Like albumin, certain immunoglobulins IgG1, IgG2 and IgG4 also bind to the FcRn (neonatal Fc receptor) and thus have a long half-life (Strohl, 2015). Similar to the fusion of albumin binding moieties, IgG binding domains (IgBDs) can be fused to therapeutic proteins. Studies have shown

different IgBDs have different affinity for serum immunoglobulins resulting in different half-lives. The longest half-life of 21 to 23 hours has been seen with the C3 domain from Streptococcal Protein G (SPG-C3) when fused to recombinant antibodies (Kontermann, 2016).

Various types of Fusion Proteins (Genetic fusion to Immunoglobulins)

In addition to evaluating multivalent NPs for the delivery of BAR peptide, we designed antibody-fused peptides to evaluate the effect of BAR valency. The antibodies acted as another carrier for the peptide. Relative to NPs, BAR fusion proteins offer the attributes of smaller size and definitive conjugation, allowing us to easily assess the impact of valency on increased binding and corresponding potency. This fusion protein allows us to begin to assess the degree of valency that is required to increase potency of the peptide to inhibit biofilms. Fusion of proteins to the Fc region of IgG 1, 2 and 4 will impart longer half-lives due to binding of FcRn (neonatal Fc Receptor) to Fc region and FcRn mediated recycling. Examples of Fc fusion proteins include TNF receptor 2 (etanercept), VEGF (vascular endothelial growth factor) receptor (aflibercept), IL-1 receptor (riloncept), CTLA-4 (cytotoxic T-lymphocyte-associated protein 4) (abatacept, belatacept) and others (Strohl, 2015). Etanercept was the first approved Fc fusion protein. Fc fusion is also used to extend the half-lives of biologically active proteins. Romiplostim, a thrombopoetin mimetic Peptide-Fc fusion protein is approved for treating immune thrombocytopenia (Kontermann, 2016) . Alprolix (Factor IX-Fc), a monomeric Fc fusion molecule, showed a terminal half-life of 57-83 hours which was approximately three times more than the half-life of other

formulations of Factor IX (Strohl, 2015). These fusion proteins and various others like Dulaglutide (GLP-1-Fc fusion protein), Efraloctocog- α (Factor VIII fused to IgG1 Fc), Corifollitropin- α (FSH-CTP fusion) have been approved for marketing (Strohl, 2015). Broadly neutralizing monoclonal antibodies (bnMAbs) may offer powerful tools as topical microbicides (Hamorsky et al., 2013). However, this option is hampered due to expensive MAb bio manufacturing based on mammalian cell culture. To address this issue, a new production system for bnMAb VRC01 in *Nicotiana benthamiana* plants using a tobamovirus replicon vector was developed (Hamorsky et al., 2013). Also, the production of antibodies using the conventional IgG production is not very safe. This novel plant based production system is being used for our experiments and employs a simple manufacturing process, as opposed to the conventional system which utilizes two separate vectors for H and L chain (Hamorsky et al., 2013). This provides a more consistent and a stable production as it generated antibodies from a single polypeptide (Hamorsky et al., 2013). We will use an IgG antibody fused to the BAR peptide to test the inhibition of interaction between *P. gingivalis* and *S. gordonii* and compare it with the soluble BAR peptide. In addition to the small size of the Ab as compared with the NPs, another reason for us to use it in our experiments is because it would allow us to be able to compare the number of BAR molecules on the NPs of the lowest BAR concentration (8.9 $\mu\text{g}/\text{mg}$ NPs) to the number of BAR molecules (2 or 4) on the BAR-Fc fusion. It would help us to determine whether or not there is a particular number of BAR molecules required to show an increase in potency.

CHAPTER 2

HYPOTHESIS AND SPECIFIC AIMS

Our overall **HYPOTHESIS** is that BAR-NPs may interact with *P. gingivalis* with higher valency than free soluble peptide, thereby increasing the avidity and potency of the interaction. This hypothesis will be tested using two approaches. The first will utilize BAR-modified NPs which can be functionalized with a high peptide valency. The second approach will examine BAR-antibody fusions with lower and more well-defined peptide valency. The Specific Aims are to:

SPECIFIC AIMS

- 1) Construct BAR-modified PLGA nanoparticles and determine whether NPs promote multivalent interaction with *P. gingivalis*.
- 2) Construct BAR-antibody fusion proteins in dimer and tetramer forms and determine if they function as more potent inhibitors of *P. gingivalis* adherence relative to free peptide

CHAPTER 3
MATERIALS AND METHODS

Peptide Synthesis

The peptide containing a covalently attached biotin at its N-terminus was synthesized by BioSynthesis, Inc. (Lewisville, TX) and was obtained with greater than 85% purity. The peptide is comprised of residues 1167 to 1193 of the SspB (Antigen I/II) protein sequence of *S. gordonii*. The BAR-Flc (Fluorescent BAR peptide) and unlabeled biotin BAR peptide used in this study, is shown in Table 1. Both contain biotin (BTN) attached to the N-Terminus and were obtained in lyophilized form.

Table 1 Sequence of BAR peptide.

Peptide Name	Peptide Sequence
BAR-Flc	(BTN)-LEAAPK- <u>K</u> flc-VQDLLKKANITVKGAFQLFS-OH
BAR	(BTN)-LEAAPK <u>K</u> VQDLLKKANITVKGAFQLFS-OH

To determine the amount of BAR peptide on the NP surface, we used the fluorescent BAR peptide (BAR-Flc) which is synthesized by covalently attaching

6-carboxyfluorescein (Flc) to the epsilon amine of the lysine residue that is underlined in Table 1.

Growth of Bacterial Strains

P. gingivalis strain ATCC 33277 was grown in Trypticase soy broth (TSBY medium) (Difco) supplemented with 0.5% (w/v) yeast extract, 1 µg/ml (final concentration) menadione, and 5 µg/ml (final concentration) hemin. Twenty milliliters of media was reduced for 24 hours under anaerobic conditions consisting of 10% CO₂, 10% H₂, and 80% N₂. Next, *P. gingivalis* was inoculated into the medium and grown for 48 hours at 37°C under anaerobic conditions. *S. gordonii* DL-1 was cultured aerobically without shaking in brain-heart infusion (BHI) broth supplemented with 1% yeast extract for 16 hours at 37°C.

Avidin-Palmitic Acid Conjugation

To obtain BAR-modified PLGA NPs, the NP surfaces were modified with avidin palmitate to subsequently attach biotinylated BAR. Avidin-palmitate was conjugated as described by Fahmy and Saltzman (Fahmy et al., 2005). Briefly, 10 mg of avidin was dissolved in 1.2 ml of 2% sodium deoxycholate (NaDC) in phosphate buffered saline (PBS) warmed to 37 °C. Palmitic acid-NHS (PA-NHS, Sigma) was dissolved in 2% NaDC at 1 mg/ml and sonicated until well-mixed. Eight hundred microliters of the 1 mg/ml PA-NHS (PA-N-hydroxysuccinamide ester, Sigma) solution was added dropwise to the reaction vial, and reacted overnight at 37 °C. The following day, the reaction was dialyzed in 1200 ml of

0.15% NaDC in PBS heated to 37 °C with 3500 MWCO dialysis tubing to remove free PA-NHS. The solution was dialyzed overnight at 37 °C, and dialysis cassette contents were transferred to a storage vial and stored at 4 °C. Two milliliters of the above made PA-NHS solution was added dropwise to the reaction vial containing avidin, and reacted overnight at 37°C. The following day, the reaction was dialyzed in 1.2L of 0.15% (w/v) NaDC in PBS. This dialysis sink solution was heated to 37°C, and a 3500 molecular weight cut off (MWCO) dialysis tube was used to remove free PA-NHS. After overnight dialysis at 37°C, complexed avidin-palmitate was transferred to a storage vial from the dialysis cassette and stored at 4°C.

Nanoparticle Synthesis

Surface-modified avidin NPs were made using the oil-in-water (o/w) single emulsion technique. On the first day, two 100 mg PLGA NP batches were each dissolved in 2 ml DCM overnight. The next day, 2 ml of 5% (w/v) polyvinyl alcohol (PVA) was mixed with 2 ml of 5 mg/ml avidin-palmitate and vortexed slowly. PLGA-DCM solution was subsequently added dropwise to two tubes that contained the previously mixed PVA-Avidin-Palmitate (4 ml) while vortexed at slow speed, with subsequent ultrasonication (Figure 3).

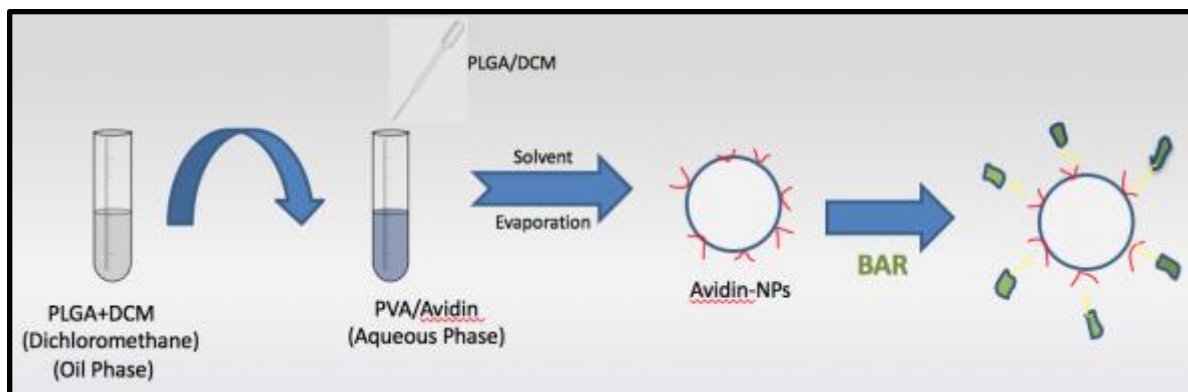


Figure 3 Oil-in-water single emulsion technique.

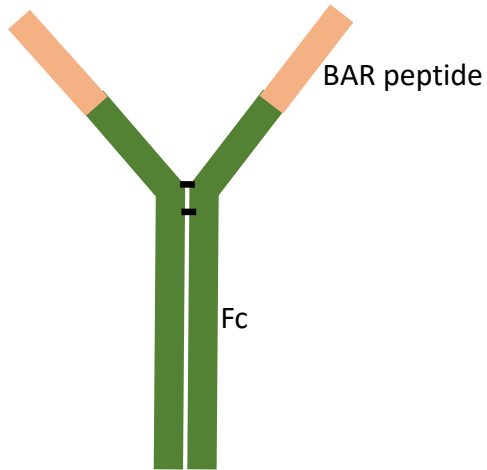
The DCM solvent was evaporated by adding the NP solution dropwise to 50 ml of 0.3% PVA and mixed for 3 hours. After evaporation, the solution was divided between six tubes and centrifuged at 13,000 rpm for 10 minutes at 4°C to wash the NPs prior to peptide conjugation. The supernatant was discarded and the pellet was suspended in 10 ml PBS. Each of the four tubes was incubated with 1 ml of BAR-Fic each at a different concentration for 1 hour. The concentrations used were 8.9, 17.8, 35.5, 71, 142 and 284 µg BAR/mg NPs, dissolved in 1 ml PBS, for a total of 10 ml reaction volume. After the reaction, NPs were transferred to centrifuge tubes, washed with 20 ml PBS and centrifuged again. The NPs were then suspended with 20 ml DI water and washed three times to remove unbound peptide. After three washes, the NPs were suspended in 5 ml of distilled water, transferred to a 10 ml cryotube, frozen in -80°C for 3 hours and subsequently lyophilized. All NPs were stored at -20°C after synthesis. The surface-modified particles with unlabeled non-fluorescent BAR peptide were synthesized similarly.

Synthesis of BAR-Fc Fusion Protein

A gene fusion protein encoding the desired Ab fused to BAR was synthesized. A chimeric rabbit human monoclonal antibody sequence was used that was designed and constructed by Dr. Palmer's team in the Owensboro Cancer Research Program. A BAR-Fc fusion dimer (Fc) (Figure 4) was constructed in which a signal peptide was fused to the BAR peptide, then fused to the IgG1 hinge and Fc region. The signal peptide is a naturally occurring secretion signal that are meant to be transported out from the cells. Once it is secreted, the protein is easy to purify. The hinge serves as a flexible spacer between the two parts of the Fc fusion protein, allowing each part of the molecule to function independently. Utilizing these motifs, enabled alterations in the fusion protein valency. Human IgG1 displays high ADCC (Antibody-dependent cell-mediated toxicity) and CDC (Complement dependent toxicity), and is the most suitable for therapeutic use against pathogens and cancer cells.

For the dimer molecule, each Fc protein has two BAR peptide molecules attached to it. In the case of the tetramer (Fc') (Figure 5), the signal peptide fused to the BAR peptide was additionally fused to both the light chain and heavy chain in place of the rabbit VL and VH sequences, resulting in a valency of four peptides conjugated to each Fc' molecule.

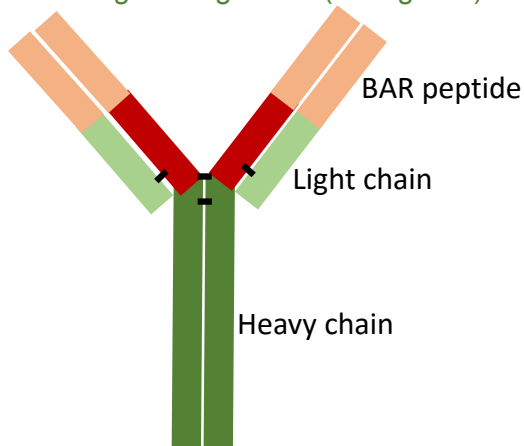
The gene was delivered via the Tobamoviral vector into *Nicotiana benthamiana* leaves. The leaf material, 5-7 days post-infiltration, was homogenized and the protein was extracted and purified. Host kex2p protease was used for cleavage to produce the antibodies in *N. benthamiana* plants.



Dimer Sequence:

MGKQMAALCGFLLVALLWLTPDVAHG-
 LEAAPKKVQDLLKKANITVKGAFQLFS-
 DKTHTCPPELLGGPSVFLFPPPKDITLMISRT
 PEVTCVVVDVSHEDPEVKFNWYVDGVEVHNAKT
 KPREEQYNSTYRVVSVLTVLHQDWLNGKEYKCKV
 SNKALPAIEKTISKAKGQPREPQVYTLPPSREEM
 TKNQVSLTCLVKGFYPSDIAVEWESNGQPENNYK
 TTPPVLDSDGSFFLYSKLTVDKSRWQQGNVFCSS
 VMHEALHNHYTQKSLSLSPGK

Figure 4: BAR-Fc fusion dimer (Fc) showing BAR peptide fused to IgG1 hinge and Fc region. Rice alpha amylase signal peptide (light blue), BAR peptide (light orange), Human IgG1 hinge + Fc (dark green)



Tetramer Sequence:

MGKQMAALCGFLLVALLWLTPDVAHG-
 LEAAPKKVQDLLKKANITVKGAFQLFS-
 RTVAAPSVFIFPPSDEQLKSGTASVVCLLNNFY
 PREAKVQWKVDNALQSGNSQESVTEQDSKD
 STYLSSTLTLSKADYEKHKVYACEVTHQGLRS
 PVTKSFNRGECGGKRTIQDSATDTVDLGAELH
 OURHOURSDDPPPTASDIGKRGG-
 LEAAPKKVQDLLKKANITVKGAFQLFS-
 ASTKGPSVFPLAPSSKSTSGGTAALGCLVKDYF
 PEPVTVSWNSGALTSGVHTFPAVLQSSGLYSL
 SSVVTPSSSLGTQTYICNVNHKPSNTKVDKR
 VEPKSCDKTHTCPPELLGGPSVFLFPPPKK
 DITLMISRTPEVTCVVVDVSHEDPEVKFNWYVD
 GVEVHNAKTKPREEQYNSTYRVVSVLTVLHQD
 WLNGKEYKCKVSNKALPAIEKTISKAKGQPRE
 PQVYTLPPSREEMTKNQVSLTCLVKGFYPSDIA
 VEWESNGQPENNYKTTPPVLDSDGSFFLYSKLT
 VDKSRWQQGNVFCSSVMHEALHNHYTQKSLS
 LSPGK

Figure 5 Fc': BAR-Fc fusion tetramer having a full antibody molecule (Fc') showing BAR peptide fused to both constant light and constant heavy chain in place of variable light and variable heavy chain. Rice alpha amylase signal peptide (light blue), BAR peptide (light orange), Constant light chain (light green), KP6 propeptide sequence (dark yellow), Constant heavy chain (dark red), Human IgG1 hinge + Fc (dark green).

Fluorescence Assay

To measure the amount of BAR peptide that was conjugated to the NP surface, a fluorescent binding assay was conducted. NPs were reacted with BAR-Flc as described above. A 1 mg/ml solution of NPs in 1X PBS was made and one hundred microliters of the suspension was added to 96-well black microtiter plates in triplicate. The fluorescence was measured at excitation/emissions wavelengths of 485 nm/535 nm, and the background fluorescence was subtracted from the final fluorescence readings. The level of BAR associated with the NP samples was determined by comparing fluorescence with a standard curve of BAR-Flc. To obtain the standard curve of BAR-Flc, a serial dilution of 1 mg/ml BAR-FLC stock was mixed with buffer to generate a range of peptide concentrations from 0.01 to 100 µg BAR peptide per ml.

Dual Species Biofilm Assay

Testing NP-BAR Inhibition

Cultures of *P. gingivalis* and *S. gordonii* were obtained as previously described. *S. gordonii* DL-1 cells were harvested by centrifuging a 19 ml culture of *S. gordonii* at 5600 rpm for 15 min. One milliliter was used to measure the initial O.D. (optical density) of cells. The supernatant was discarded and the cell pellet was suspended in 1 ml of 1X PBS. *S. gordonii* was labeled with 40 µl of 5 mg/ml hexidium iodide (Molecular Probes, Eugene, OR) and incubated for 15 min at room temperature on a rocker platform protected from light. After incubation, the labeled samples were centrifuged at 10,000 rpm for 3 mins, the supernatant was

discarded, and the cells were suspended in 1 ml of 1X PBS. Following this, the O.D. was measured at 600 nm from twenty-fold diluted cultures of *S. gordonii* to determine cell count. For all experiments, the optical density of *S. gordonii* cells was adjusted to 0.8 for uniformity of the *S. gordonii* cell counts in each well. After adjusting the optical density, 1 ml of *S. gordonii* cells was added to each well of five 12-well culture plates containing a sterilized micro-coverslip. The cell culture plates were wrapped in aluminum foil to protect the labeled cells from light and placed on a rocker platform in the anaerobic chamber for 24 hours.

P. gingivalis cultures used for biofilm formation were optimized using a similar approach. In short, 19 ml of *P. gingivalis* cells were centrifuged for 15 min at 5600 rpm and 1 ml was used to measure the initial O.D. The supernatant was discarded and the cell pellet was suspended in 1 ml of pre-reduced 1X PBS. *P. gingivalis* cells were labeled with 40 μ l of 4 mg/ml carboxyfluorescein-succinylester (Molecular Probes). Cells were incubated with the fluorescent dye for 15 mins on a rocker platform and protected from light. Following incubation, cells were centrifuged at 10,000 rpm for 3 min and the supernatant was discarded to remove the unbound fluorescent dye. The pelleted cells were suspended in 1ml of pre-reduced 1X PBS. The optical density of *P. gingivalis* cells was adjusted to 0.4 for uniformity of the *P. gingivalis* cell counts in each well.

For biofilm inhibition experiments, BAR-NPs, soluble BAR or avidin-only NPs were pre-incubated with labeled *P. gingivalis* at 25°C for 30 min before transferring to the appropriate wells. The NPs that were surface-modified with

unlabeled BAR peptide were used for these experiments. For each batch of NPs that were synthesized, using input concentrations of BAR of 71 µg BAR/mg NPs, 35.5 µg BAR/mg NPs, 17.8 µg BAR/mg NPs, or 8.9 µg BAR/mg NPs, five different concentrations of BAR (0.3 µM, 0.7 µM, 1.3 µM, 2.0 µM, 2.5 µM) were tested for biofilm inhibition. After calculating the amount of NPs required to deliver the desired level of BAR peptide, one milliliter of each of these solutions was added in triplicate to the culture plates. Molar equivalents of free BAR peptide (0.3 µM, 0.7 µM, 1.3 µM, 2.0 µM, 2.5 µM) were also tested. Controls comprised treating cells with PBS alone or with avidin-only NPs in triplicate. The cell culture plates were covered with aluminum foil and incubated for 18-24 hours in an anaerobic chamber.

Following incubation, the supernatant was removed from the wells of the cell culture plates and the cells were washed with pre-reduced 1X PBS to remove non-adherent bacterial cells. The cells were subsequently fixed with 4% (w/v) paraformaldehyde, excess paraformaldehyde was removed, and the cells were washed with pre-reduced 1X PBS. After washing, the coverslips were mounted on a glass slide using Prolong Gold anti-fade reagent and viewed using confocal laser scanning microscopy.

Testing BAR-Fc Fusion Inhibition

Biofilm inhibition by the purified BAR-Fc fusion protein was conducted similarly as described above. Three different concentrations of the BAR-Fc fusion protein were tested; 1 µM, 0.5 µM, and 0.25 µM, corresponding to 2.0 µM, 1.0 µM and

0.5 μM equivalents of BAR, respectively, since each fusion protein contained two molecules of BAR. Free BAR-peptide (unlabeled) at concentrations of 2.0 μM , 1.0 μM and 0.5 μM were tested. Control reactions consisted of treating cells with PBS alone or with antibody that did not contain BAR.

Confocal Microscopy

P. gingivalis-*S. gordonii* biofilms were visualized using a Leica Microsystems confocal laser scanning microscope (TCS SP8) and the Leica Application Suite X software. The slides were viewed using an argon laser for visualization of FITC-labeled *P. gingivalis* and the HeNe-G laser to visualize hexidium iodide-labeled streptococci. *P. gingivalis* binding was determined from randomly chosen frames using Leica Application Suite X Software. Z-stack images of the biofilms were obtained using a z-step size of 0.7 μM and were constructed and analyzed using the Volocity image analysis software.

Image Analysis

After obtaining biofilm images using confocal microscopy, the resulting z-stack images were processed and reconstructed into 3D images using the Volocity software. Images were imported into Volocity as multiple Tiff-files. Uniform filters were used to remove noise from the images and were further analyzed to quantify the extent of *P. gingivalis* binding. The image brightness and contrast was adjusted equally for all frames, and a snapshot of the image was captured. Next, the ratio of green to red fluorescence was determined. Each peptide

concentration was analyzed in triplicate and 3 independent frames were measured for each well. The mean and variation (SD) between samples was determined using ANOVA. The variation was considered statistically significant when $P < 0.05$.

CHAPTER 4

RESULTS

Surface Modification Efficacy of PLGA NPs with BAR Peptide

A fluorescence assay was used to determine the amount of BAR peptide that was bound to the surface of the NPs. Avidin-NPs were titrated with BAR peptide at six different concentrations; 8.9, 17.8, 35.5, 71, 142 and 284 μg BAR/mg NPs. Previous experiments showed that a concentration of 142 μg BAR/mg NPs was required to saturate the available avidin binding sites. However, in those experiments 2 ml of 5 mg/ml avidin was used to modify 50 mg PLGA NPs during synthesis. In the current experiments, 2 ml of 5 mg/ml avidin was used to modify 100mg PLGA NPs, resulting in half the modification density (per mg NP) used in previous experiments. To measure the degree of modification, NPs were incubated with various concentrations of BAR-FIc for 1 hour, washed, frozen, and lyophilized. Fluorescence was measured as previously described. We observed that the incorporation of BAR-FIc was directly related to the concentration of BAR-FIc added. A standard curve (Figure 6) of soluble BAR-FIc was used to quantify the output concentration of BAR.

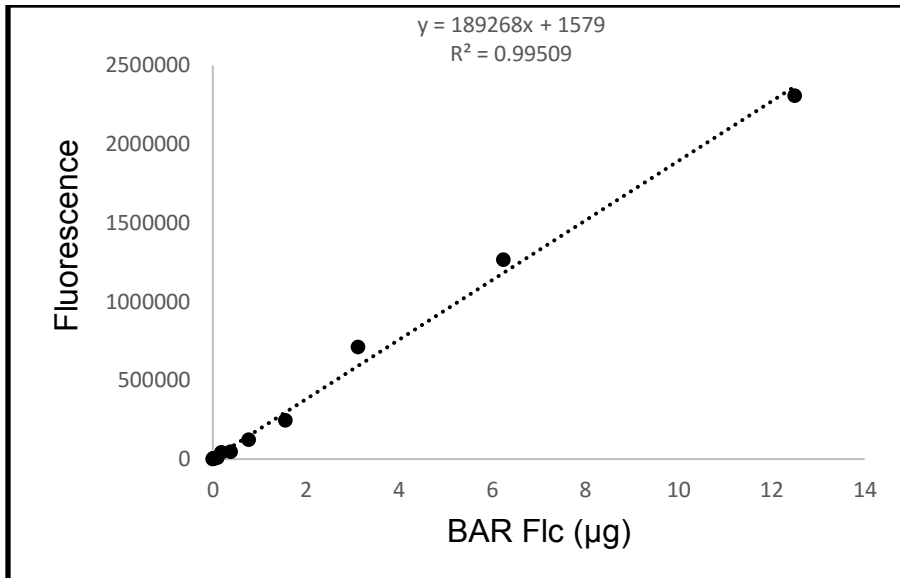


Figure 6 Standard Curve for free BAR peptide showing fluorescence at increasing BAR amounts. This graph was used to calculate the BAR FIC output concentration for the BAR-NPs. The x-axis is expressed in terms of the amount of BAR added per well (µg).

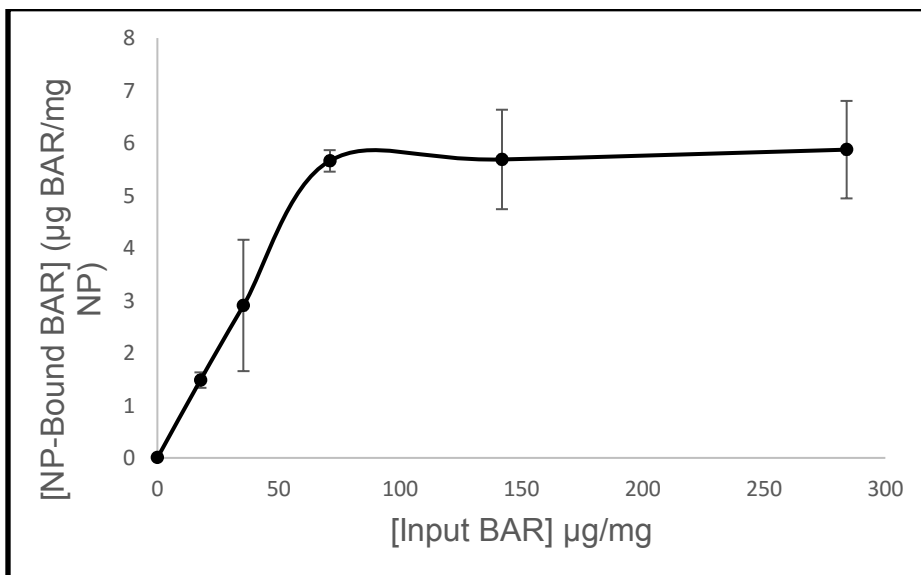


Figure 7 Saturation curve for fluorescently labelled BAR. The input concentration of BAR was varied and resulted in a dose-dependent amount of BAR conjugated to the NP surface ranging from 1.48 to 5.87 µg BAR/mg NPs. We observed that above 71 µg BAR/ mg NP (input concentration), the avidin sites on the NP surface were saturated resulting in no additional conjugation to the NP surface.

As shown in Figure 7, an input concentration of 71 $\mu\text{g}/\text{mg}$ NPs resulted in saturation, indicating that all available avidin binding sites were bound by biotin-BAR peptide. Beyond this input concentration, additional peptide was not conjugated to the NP surface.

Table 2 Correlation between the input concentration of BAR-FLC peptide and quantity of BAR-FLC on the NP surface. Increasing amounts of BAR peptide resulted in increased amounts of conjugated BAR. However, above 71 μg BAR/mg NP, the NP surface was saturated as seen in Figure 7.

Sample	[Input: Quantity of BAR-Flc peptide (μg) reacted with surface of NPs (mg), $\mu\text{g}/\text{mg}$]	[Output: Quantity of BAR-Flc peptide (μg) bound to surface of NPs (mg), $\mu\text{g}/\text{mg}$]
A	284	5.87 \pm 0.48
B	142	5.69 \pm 0.95
C	71	5.66 \pm 0.20
D	35.5	2.90 \pm 0.16
E	17.8	1.48 \pm 0.17
F	8.9	1.20 \pm 0.68

Previous experiments showed incorporation of 1.5 nmol avidin per mg NP.

Assuming 4 binding sites per avidin, the maximal payload of BAR is 6 nmol per mg NP (\sim 22 $\mu\text{g}/\text{mg}$ NP). According to Table 2, after reacting the NP surface with

71, 142, and 284 μg BAR/mg NPs, the NP surface was saturated with BAR peptide, and bound approximately 5.7 μg BAR per mg NP. This suggests that 26% of the avidin binding sites are available for interaction with BAR.

Biofilm Inhibition Assay with BAR-NPs

The biofilm inhibition and fluorescence binding assays were performed in parallel to minimize experimental errors. As previously discussed, different concentrations of BAR-NPs were evaluated to determine the effect of peptide valency on *P. gingivalis* and *S. gordonii* inhibition. Streptococcal cells were immobilized and *P. gingivalis* was incubated with *S. gordonii* for 18-24 hours. The biofilms were visualized using confocal microscopy and the percent inhibition was calculated by determining the ratio of *S. gordonii* to *P. gingivalis* cells using Volocity. Previous studies showed that the IC_{50} (50% inhibitory concentration) of soluble BAR was 1.3 μM ; therefore, a range of BAR molar equivalents ranging from 0.3 - 2.5 μM was tested for each formulation of BAR-NPs (containing payloads of 1.20, 1.48, 2.90 and 5.66 μg BAR/mg NP; see Table 2). For control reactions, *P. gingivalis* was treated with defined concentrations of soluble BAR (1.3, 2.0, and 2.5 μM) or avidin-NPs alone. *P. gingivalis* was also incubated with *S. gordonii* in the presence of buffer alone. The corresponding biofilm images are shown in Figures 8 and 9.

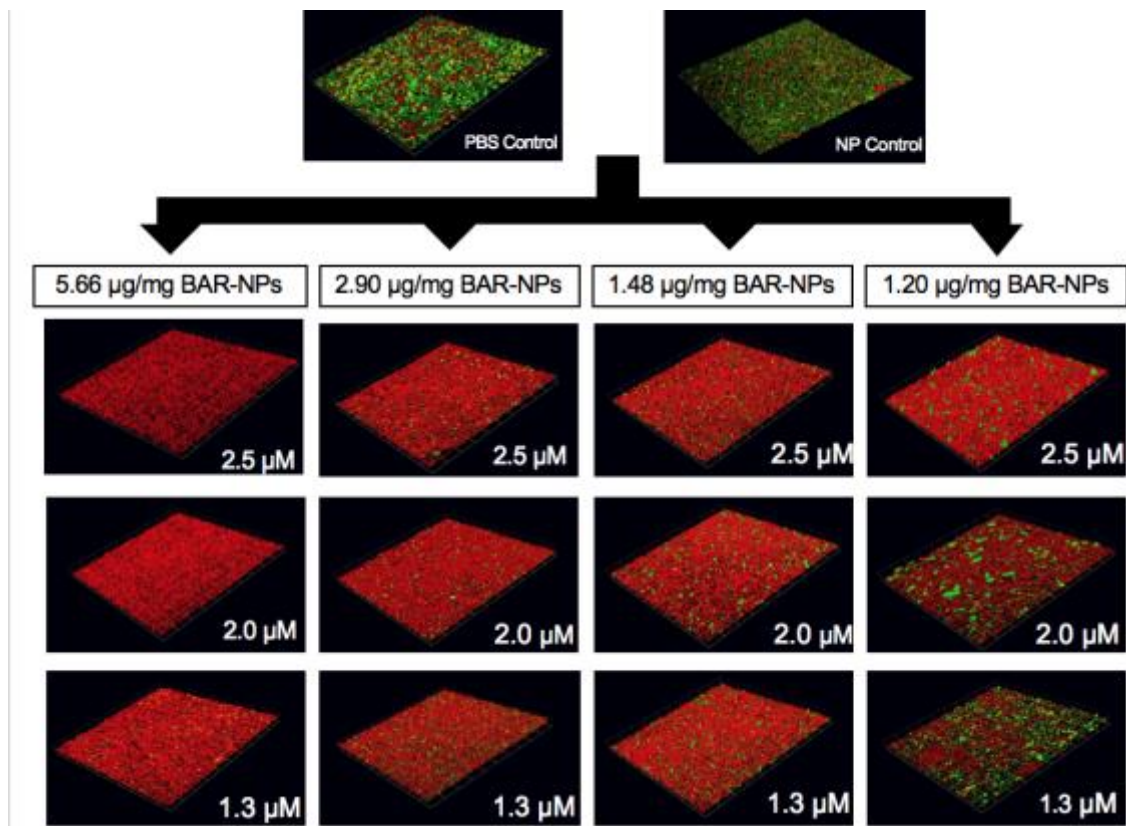


Figure 8: BAR-NP inhibition of *P. gingivalis* (green cells) adherence to *S. gordonii* (red cells). Biofilms were visualized by confocal microscopy and image stacks were assembled using Volocity image analysis software. The concentrations indicated on the images represent BAR peptide equivalents on the NP surface. As the surface density of BAR on the NP surface decreases (left-to-right), a decrease in biofilm inhibition is observed, indicated by the increased presence of *P. gingivalis* cells (green). Similarly, as the molar equivalent of BAR peptide delivered by each NP formulation is decreased (top-to-bottom), we observe a decrease in biofilm inhibition indicated by the increased presence of *P. gingivalis* cells (green). This figure displays molar equivalents of BAR ranging from 2.5 to 1.3 μM .

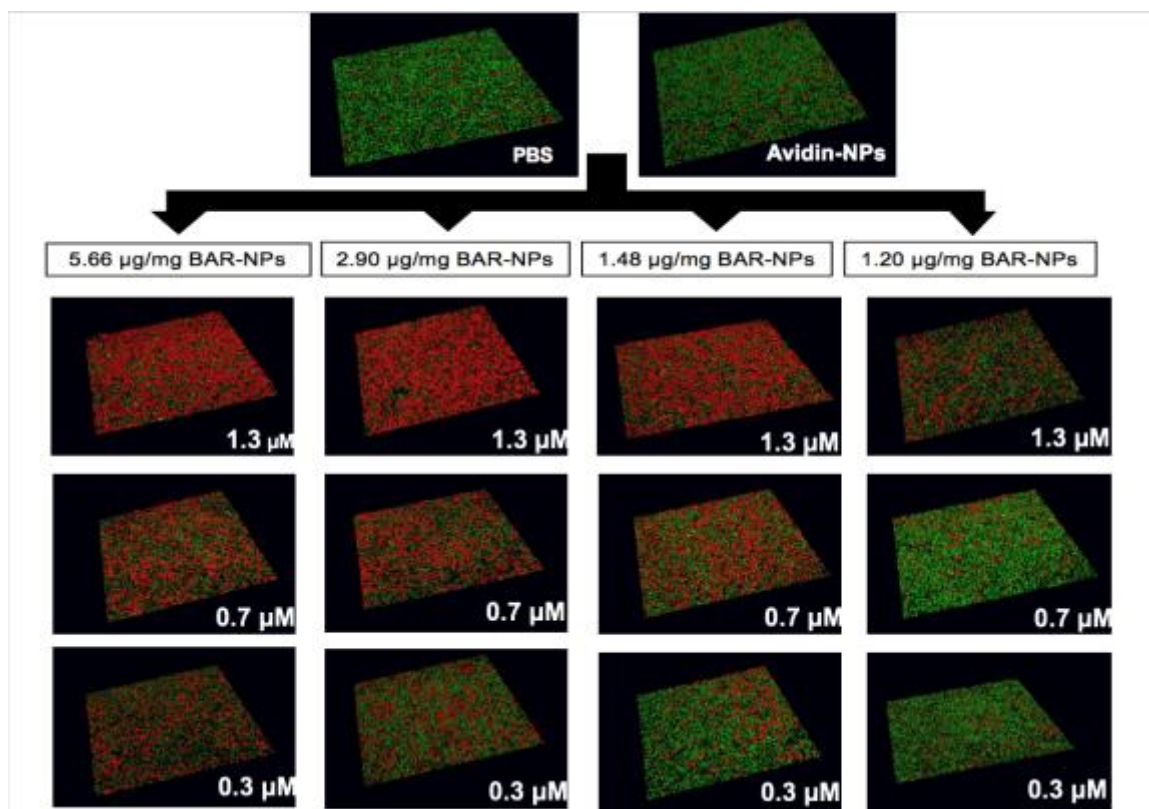


Figure 9: BAR-NP inhibition of *P. gingivalis* (green cells) adherence to *S. gordonii* (red cells). Biofilms were visualized by confocal microscopy and image stacks were assembled using Volocity image analysis software. The concentrations indicated on the images represent BAR peptide equivalents on the NP surface. As the surface density of BAR on the NP surface decreases (left-to-right), a decrease in biofilm inhibition is observed, indicated by the increased presence of *P. gingivalis* cells (green). Similarly, as the molar equivalent of BAR peptide delivered by each NP formulation is decreased (top-to-bottom), we observe a decrease in biofilm inhibition indicated by the increased presence of *P. gingivalis* cells (green). This figure displays molar equivalents of BAR ranging from 1.3 to 0.3 μM .

Robust formation of *P. gingivalis*/*S. gordonii* biofilms occurred in the PBS and avidin-NP control reactions, whereas significant inhibition of biofilm formation was seen when cells were incubated with the BAR-NP preparations. This indicates that NPs without BAR have no effect of *P. gingivalis* adherence to streptococci and subsequent biofilm formation and that inhibition of biofilm

formation can be attributed to BAR peptide delivered by NPs.

The biofilm images were organized horizontally from left to right (see Figures 8 and 9) with the NP formulation containing the highest payload of peptide (5.66 $\mu\text{g}/\text{mg}$ NP) on the left and lowest payload (1.20 $\mu\text{g}/\text{mg}$ NP) on the right. In each vertical columns, the molar equivalent of BAR peptide delivered by each NP formulation is decreased. As shown in Figures 8 and 9, the biofilm inhibition increased with increasing BAR payload, even though each NP preparation delivered the same molar equivalent of BAR peptide.

This suggests that BAR-NPs with higher payloads interact with *P. gingivalis* at higher valency. In addition, as expected a dose dependent inhibition of biofilm formation occurred as the molar equivalent of peptide delivered by the various NP formulations was increased. Table 3 summarizes the percent biofilm inhibition calculated for each NP formulation and for each molar equivalent of BAR that was tested.

Table 3 Maximum biofilm inhibition is observed for NPs functionalized with the highest valency of BAR peptide. Biofilm inhibition decreases as a function of NP valency and total BAR concentration.

Sample valency (μg BAR/mg NPs)	[BAR] μM	% Inhibition
5.66	2.5	94.15
	2	92.00
	1.3	88.6.0
	0.7	61.82
	0.3	30.70
2.90	2.5	80.96
	2	77.91
	1.3	75.45
	0.7	39.93
	0.3	29.41
1.48	2.5	68.30
	2	65.08
	1.3	63.58
	0.7	40.48
	0.3	24.71
1.20	2.5	59.83
	2	52.92
	1.3	43.12
	0.7	17.05
	0.3	14.93

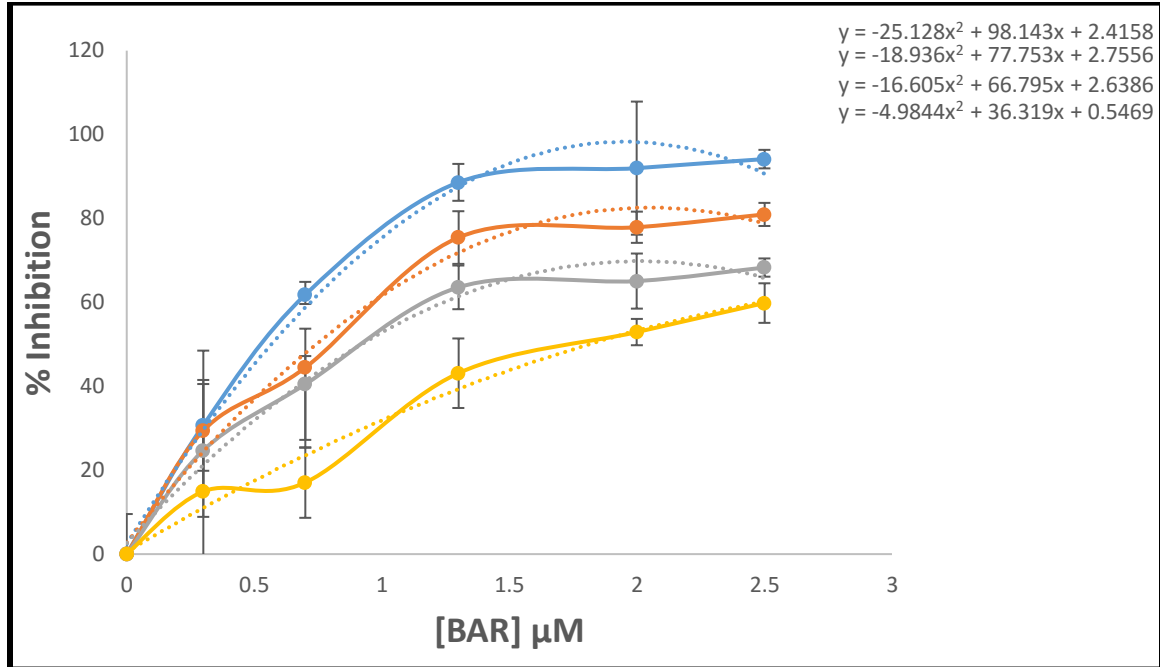


Figure 10 Biofilm inhibition curves showing BAR concentration versus percent inhibition for each NP surface modification group. Percent inhibition for 5.66 (blue), 2.90 (orange), 1.48 (grey) and 1.20 (yellow) μg BAR/mg NP are shown.

Overall, the NPs with the highest peptide valency exhibited the lowest IC_{50} values (Table 4). Conversely, as the valency of the BAR-NPs decreased, the IC_{50} value increased (Figures 10 and 11). The BAR-NPs bound to *P. gingivalis* significantly inhibited *P. gingivalis*-*S.gordonii* interaction as compared with PBS and avidin-NPs controls ($p < 0.05$).

To determine the number of peptides corresponding to NP valency for the different formulations, the number of BAR peptides on each NP was calculated as a function of NP size, diameter, peptide MW, and conjugation density. The concentration of peptide conjugated per milligram NP: 5.66, 2.90, 1.48 and 1.20 μg BAR/mg NPs (Table 2), corresponded to 2140, 1089, 556 and 451 peptides

per NP, respectively.

Table 4 As the input BAR concentration decreases, the IC_{50} increases

Sample	Input BAR concentration $\mu\text{g}/\text{mg}$ NPs	Output BAR concentration $\mu\text{g}/\text{mg}$ NPs	IC_{50} μM
A	71	5.66	0.56
B	35.5	2.90	0.74
C	17.8	1.48	0.91
D	8.9	1.20	1.81

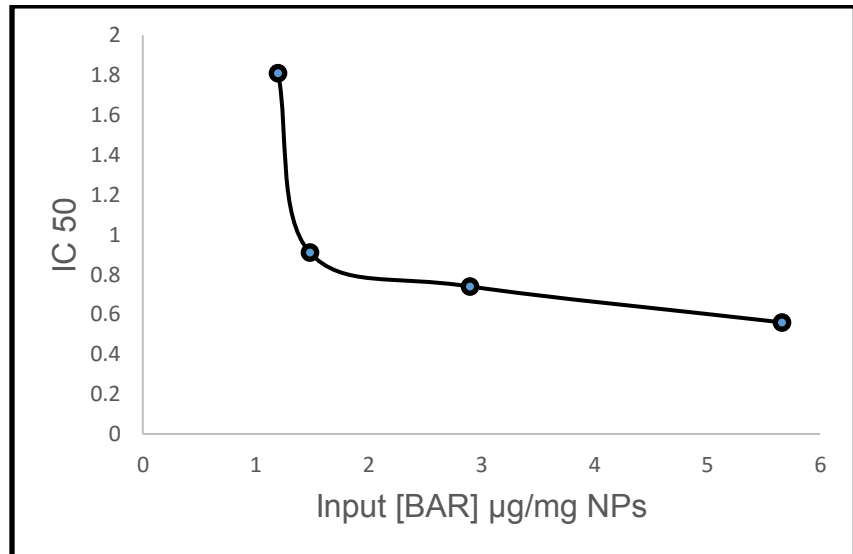


Figure 11 The lowest IC_{50} is achieved in the sample with the highest valency of BAR peptide.

Biofilm Inhibition Assay with BAR-Fc Fusion

The BAR-Fc fusion biofilm inhibition assay was conducted similar to the BAR-NP experiment. The BAR-Fc fusion concentrations (dimer) used to determine biofilm inhibition were 0.25, 0.5, and 1 μM BAR-Fc. For control reactions, *P. gingivalis* was treated with defined concentrations of soluble BAR (0.5, 1.0 and 2 μM). Control reactions consisted of *P. gingivalis* incubated with Ab alone or with buffer alone. The biofilm images along with the controls are shown in Figure 12. In addition to synthesizing the dimer fusion protein, we attempted to synthesize a tetramer fusion protein. During the synthesis process, there were challenges in the expression and purification of protein. Future experiments will seek to address this issue.

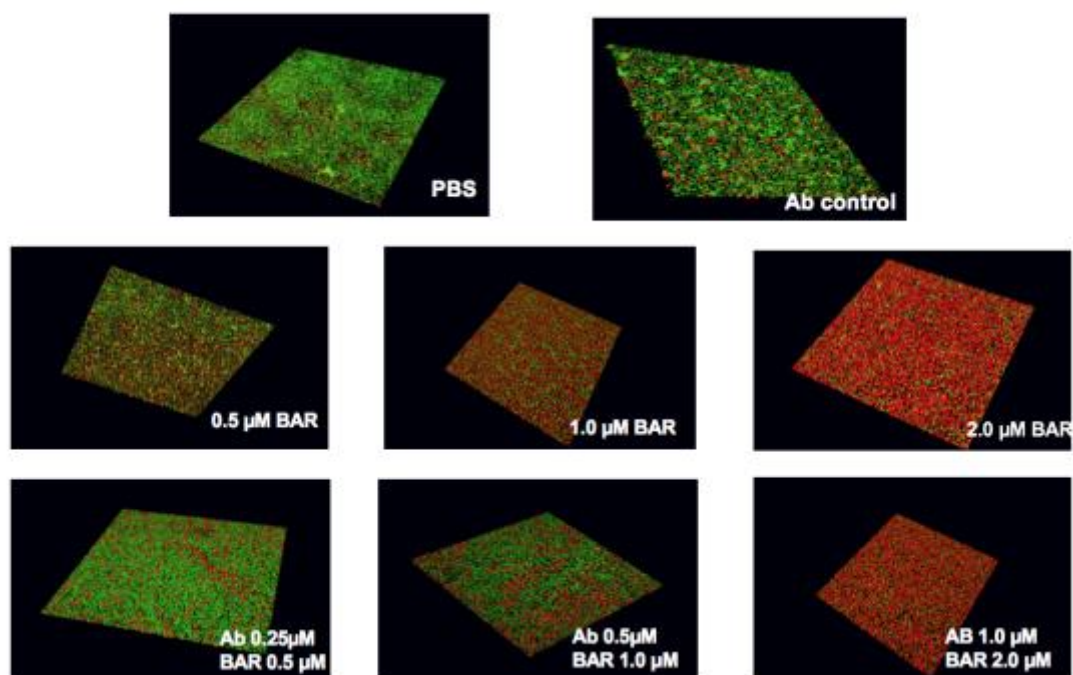


Figure 12 BAR-Fc inhibition of *P. gingivalis* adherence to *S. gordonii*. Biofilms were visualized by confocal microscopy and image stacks were assembled using Volocity image analysis software. Red cells represent *S. gordonii* and green cells represent *P. gingivalis*. The concentrations indicated on the images represent BAR peptide equivalents conjugated to the antibody.

Figure 12 shows that as the amount of BAR peptide is increased from 0.5 μM (Ab=0.25 μM) to 2 μM (Ab=1 μM), there is a decrease in the number of *P. gingivalis* cells (green cells) adhered to streptococci and increased inhibition of biofilm formation. As shown in Table 5, a dose-dependent increase in the percent inhibition of biofilm formation occurred as the amount of the BAR peptide increased.

Table 5 A BAR-Fc fusion protein containing two molar equivalents of BAR was synthesized and tested against free peptide for biofilm inhibition. The table shows the input BAR amount versus percent inhibition for increasing concentrations of peptide in Ab-BAR fusion proteins. Percent inhibition was calculated by quantifying fluorescence of the confocal images and plotted against the equimolar amounts of BAR peptide present in each sample of the BAR-Ab fusion proteins. A dose-dependent response was observed.

Sample	Input BAR amount (μM)	Percent Inhibition
A	0.5	10.77
B	1.0	28.73
C	2.0	63.78

Table 6 shows that the IC_{50} for the Ab-BAR fusion peptide was approximately 1.6 μM which is similar to the IC_{50} of free BAR peptide. This indicates that for this particular formulation, the Ab-BAR fusion peptide was not more potent than soluble BAR peptide ($p < 0.05$).

Table 6 The IC_{50} of interaction for the Ab-BAR Fusion protein was determined to be 1.61 μM which is similar to that of free BAR peptide

Peptide	IC 50
BAR	1.3 μM
Ab-BAR Fusion	1.6 μM

*Daep C.A., R.J. Lamont and D.R. Demuth. 2008. 576

CHAPTER 5

DISCUSSION

While the oral cavity accommodates both anaerobic and aerobic organisms, the environment of the oral cavity poses an adverse environment for organism survival (Dalwai et al., 2006). Due to the action of saliva, which reduces the accumulation of bacteria by various mechanisms, the bacteria must struggle to survive and stay in the oral cavity (Dalwai et al., 2006). To counteract the effects of saliva, the initial colonization and adhesion of bacterial organisms to the tooth surface occurs via the acquired pellicle (Lindh et al., 2014). Subsequent bacterial adhesion and colonization occur with the help of contact-dependent signaling, leading to the initiation and development of polymicrobial biofilms (Donlan, 2002). These polymicrobial biofilms are comprised of a structured community of microorganisms that are adhered to the surface and enclosed in a self-generated matrix. Interaction within these biofilms can be mutualistic, commensalistic or antagonistic (Willems et al., 2016). These interactions contribute to the formation of subgingival biofilms that stimulate a cascade of chronic inflammatory reactions by the diseased tissue (Bao et al., 2014). Its initiation is attributed to the formation of subgingival biofilms that stimulate a cascade of chronic inflammatory reactions by the diseased tissue (Bao et al., 2014). *Porphyromonas*

gingivalis, *Tannerella forsythia* and *Treponema denticola* are associated with the occurrence and severity of the disease and are found as a part of these biofilms (Bao et al., 2014). *P. gingivalis* is one of the 'red' complex bacteria and has been suggested to function as a keystone pathogen (Darveau et al., 2012). *P. gingivalis* can be cultivated easily and genetic tools are available to facilitate its study (Suzuki et al., 2013). For these reasons *P. gingivalis* has been extensively studied and is being targeted as a key organism to inhibit biofilm formation (Darveau et al., 2012; Suzuki et al., 2013). Mechanistically, *P. gingivalis* is an obligate anaerobe and its primary niche is the subgingival pocket, but before it can establish itself there it must survive within the relative aerobic supragingival pocket. To enable its survival, *P. gingivalis* interacts with a facultative anaerobe *S. gordonii* supragingivally. This interaction is an initial event in biofilm formation, and represents an ideal target to inhibit the colonization of *P. gingivalis* and combat the initial stages of periodontitis. (Daep et al., 2008; Darveau et al., 2012; Park et al., 2005).

The interaction between *S. gordonii* and *P. gingivalis* involves the Mfa1 of *P. gingivalis* binding to the SspB of *S. gordonii* (Cook et al., 1998; Daep et al., 2006; Park et al., 2005). Previous studies have suggested a specific region on SspB that is involved in the interaction (Daep et al., 2006). This area has been recognized as BAR (Ssp**B** Adhering **R**egion) and studies have led to the development of a peptide (BAR) which is derived from the antigen I/II protein of *S. gordonii* (Daep et al., 2006; Daep et al., 2008). BAR peptide has demonstrated potent inhibition of *P. gingivalis* adherence to *S. gordonii*. BAR

also significantly reduced *P. gingivalis* virulence in mice which harbored *S. gordonii* and were subsequently inoculated with *P. gingivalis*. (Daep et al., 2011). Additionally, BAR peptide proved potent in a dual-species biofilm; however, its efficacy decreased in pre-formed and more complex biofilms, requiring increased quantities and longer duration of peptide incubation (Gummadi, 2013, unpublished). In efforts to improve potency and to achieve a concentrated dose of BAR at the target site, surface-modified multivalent BAR-PLGA NPs were constructed.

The consideration of multivalency in the design of therapeutic carriers has the potential to enhance the inhibitory potential of low affinity molecules by increasing the number of interactions and decreasing the dissociation rates (avidity), between the delivery carrier and its therapeutic binding target. (Chittasupho, 2012). Multivalent approaches have proven effective to block the attachment of the influenza virus to its target cell by an inhibitor which is multivalent (Mammen et al, 1998). Similarly, multivalent targeting approaches amplified angiotensin II receptor type 1 blockade in the eye and concomitantly deliver a therapeutic payload into ocular lesions. In this project we implemented the concepts of multivalency to create high avidity interactions between the BAR-modified NPs and the bacterial binding receptors. We hypothesized that carriers with increased valency would increase the potency of the peptide (Chittasupho, 2012).

Nanoparticle technology has contributed to a variety of translational applications,

demonstrating versatility and biocompatibility in the delivery of an assortment of cargo, including drugs, genes, and proteins. Recently, NPs have found use in various areas of restorative dentistry, minimally invasive dental procedures, cancer diagnosis and treatment, molecular imaging and implant dentistry (Mantri & Mantri, 2013). Due to their high structural integrity, stability during storage, ease of preparation and functionalization, and controlled release capability, polymeric NPs are highly attractive as drug delivery vehicles (Cheow & Hadinoto, 2014).

Recent studies employing NPs for oral applications, have shown that BAR-NPs are more potent than the soluble BAR in inhibiting *P. gingivalis* adherence to *S. gordonii*, and preventing biofilm formation (Steinbach-Rankins, Demuth, unpublished). In this work, NPs were surface-modified with avidin to bind to the biotin of the BAR peptide. Avidin-biotin-ligand conjugation is considered to be one of the strongest non-covalent bonds and offers an efficient method of attaching the peptide to the NP surface (Bratthauer, 2010; Howarth et al., 2006). It was determined that each avidin has four biotin binding sites, but due to their close proximity to each other, leading to steric hindrance, we assumed that only two of the biotin-binding sites were available for biotinylated BAR conjugation (Howarth et al., 2006; Steinbach et al., 2016). The mechanism by which the PLGA-NPs enhanced the potency of the BAR peptide may be due to increased localized concentration of the BAR peptide or by promoting a multivalent binding interface to increase the avidity of BAR with *P. gingivalis*. In our experiments we hypothesized that BAR-NPs increased the avidity of the interaction by increasing

the valency of BAR, thereby increasing the potency relative to free BAR peptide. We used two experimental assays to evaluate the efficacy as a function of increased BAR valency. Biofilm inhibition assays were performed using BAR-NPs and BAR-Fc fusion proteins, and the percent inhibition of *P. gingivalis* to *S. gordonii* adherence was compared to that of free BAR peptide.

First a direct approach was used to quantify the amount of BAR bound to the NP surface. BAR-Fc was reacted with NPs at concentrations of: 8.9, 17.8, 35.5, 71, 142, and 284 μg BAR/mg NPs. We varied these concentrations around a three-fold molar excess of BAR (71 μg BAR/mg NPs) to available binding sites and observed that at this concentration, all available avidin binding sites were saturated on the NP surface. The percentage of BAR bound to the NPs, relative to the input concentration remained constant (24%) even upon increased concentrations of reactant BAR (e.g. 142 and 284 μg BAR/mg NPs). In comparison with previous experiments, in which the same amount of avidin was added to 100 mg versus 50 mg PLGA NPs, half the amount of BAR was needed (71 vs. 142 μg) indicating that less avidin may be used during the synthesis process to induce similar binding results. In our experiments, we achieved 1.20 ± 0.68 , 1.48 ± 0.17 , 2.90 ± 0.16 , and 5.66 ± 0.20 μg BAR/mg NPs, bound to the NP surface at input concentrations of 8.9, 17.8, 35.5, and 71 μg BAR/mg NPs, respectively, demonstrating very efficient binding.

To determine if this increase in the binding efficiency was attributed to an increase in valency, similar concentrations of BAR-NPs (8.9, 17.8, 35.5, 71, 142, and 284 μg BAR/mg NPs) were reacted with *P. gingivalis*. *P. gingivalis* cells

were subsequently incubated with immobilized *S. gordonii* to form biofilms. Five different equimolar BAR peptide concentrations (0.3, 0.7, 1.3, 2.0, and 2.5 μM) for each batch of BAR-NPs (with differing valency) were evaluated. As the equimolar BAR NP concentration increased, biofilms were increasingly inhibited and *P. gingivalis* to *S. gordonii* interaction decreased. We also found out that the 50% inhibitory concentration was highest for the BAR-NP sample that had the maximum BAR density (valency) on the NP surface.

Next, we used a different platform to deliver BAR peptide – a BAR -Ab fusion protein. IgG was used in a dimer form and BAR peptide was fused to it using a novel plant based production platform, with one molecule of antibody carrying two molecules of BAR (Hamorsky et al., 2013). The biofilms were formed using a concentration range of BAR: 0.5 μM (Ab=0.25 μM), 1 μM (Ab=0.5 μM), and 2 μM (Ab=1 μM), and biofilm inhibition was quantified. Although a linear increase in the percent inhibition was observed as the amount of BAR peptide increased, the IC_{50} (1.6 μM) was similar to that of free BAR alone (IC_{50} =1.3 μM). Hence, to make the BAR-Fc fusion more potent, we believe that more BAR molecules need to be fused per Ab molecule. As we calculated before, 451 molecules of BAR are present per NP in 8.9 μg BAR/mg NP (lowest valency) batch as compared to 2 molecules in a BAR-Fc fusion, it is not surprising that we did not see an increase in potency of BAR in BAR-Fc fusion proteins. Our data, therefore, suggests that increased number of BAR molecules are required to improve the fusion protein potency. We also speculate that if the tetramer form of BAR-Fc fusion (Fc') were to be tested, we would not have been able to observe an increase in the potency

of that particular formulation as we believe that more than 2 but less than 451 molecules of BAR are required to achieve the desired effect. This comparison highlights differences between platforms that enable low, relative to high density modification; however, we acknowledge that there are likely differences in available BAR spatial arrangements between NP and Ab carriers. Therefore, even equivalent amounts of BAR on each carrier may exhibit dissimilar effects in binding, due to platform differences.

This concept of the increased percent inhibition due to an increase in valency, provides us a solid framework to develop therapeutics, by designing NPs to specifically target microorganisms more effectively and safely. As recent studies suggest that *P. gingivalis* plays a significant role in altering the host-microbe homeostasis, new delivery platforms for BAR peptide seek to block *P. gingivalis* interactions more effectively. We understand that the etiology of periodontitis is very complex and there might be many more bacterial interactions simultaneously involved, which might have significant impact on disease progression. The surface-modified NPs could, therefore, be applied to target other bacterial interactions in the oral cavity and combat the bacterial colonization, thereby, periodontitis. This could be achieved by modifying the NPs with peptides pertaining to particular interactions.

The experimental results suggest that by increasing NP valency, we can obtain increased avidity and potency of the peptide. This paves the way for lower concentrations of BAR to be used, while still achieving similar efficacy. Constant flow of saliva in the oral cavity and the intake of food and water may regularly

wash out the therapeutic peptides (BAR) which would decrease the effectiveness of BAR. Due to the efficacy of BAR-NPs at both high and low concentrations, relative to free BAR peptide, this approach may prove very beneficial. Since BAR peptide is relatively expensive to produce, this method of conjugating BAR to NPs may offer a more cost effective alternative for delivery. Additionally, because of the conjugation with NPs, BAR can be delivered locally in a concentrated form to increase BAR effectiveness. For translational applications, BAR-modified NPs may, eventually, be prescribed as mouthwashes or chewing gums after oral prophylaxis procedures done in a dental office. This would offer a cure for periodontitis and not just a preventive treatment like scaling or gingival surgery.

We are still establishing effect of BAR-modified NPs on pre-formed and more complex biofilms. Future directions of this research project will study the effect of BAR-NPs in established biofilms as well as in more complex biofilms with *Fusobacterium nucleatum*, *in vitro*. From a design perspective, decreased avidin reactant may be used for conjugation to the NP surface, which may further increase the potency of the BAR peptide. Experiments will also be conducted to determine the toxicity of surface-modified NPs in human gingival cells, with eventual translation to animal models. Regarding BAR-Fc fusion proteins, additional modifications of the non-Fc binding BAR Abs will be pursued to enhance their therapeutic potential. For example, they may be constructed in tetramer or higher valency forms, which would incorporate four or more molecules for BAR per molecule of Ab. These formulations may prove promising

for inhibition. To benefit from both delivery technologies, we may investigate Ab-BAR-NPs, to enhance and prolong effects in the oral cavity. Our long-term goal is to develop a therapeutic that can be approved to be tested in clinical trials. We envision that clinical trials will require recognizing that the oral cavity is a niche for many organisms. This would involve creating conditions that would harbor only the bacteria that need to be studied. We envision that clinical prevention and treatment may involve the administration of BAR peptide immediately after oral prophylaxis. With this, the number of *P. gingivalis* cells that recolonize the oral cavity with time can be used as an outcome to assess the efficacy of BAR-NP preparations. For example, one possible approach is to subject patients to oral prophylaxis and then provide one group with a mouth rinse containing BAR-NPs and a second group with a placebo formulation. The kinetics of *P. gingivalis* recolonization would serve as the outcome to determine the effectiveness of the treatment protocol. In these experiments, patient compliance must be monitored very carefully. Overall, BAR-NPs look very promising and may pave the way to develop therapeutics that would actually prevent biofilms from forming and thereby reducing the incidence of chronic periodontitis.

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CURRICULUM VITAE

NAME: Ankita Jain

ADDRESS

Dept. of Oral Immunology and Infectious Disease
University of Louisville School of Dentistry
501 South Preston Louisville, KY 40202

DOB

Khanna, Punjab State, India. – June 20, 1987

EDUCATION & TRAINING

B.D.S, Dental Surgery
Himachal Pradesh University
2005-2010

DENTAL EXPERIENCE

Associate Dentist – Dabur Dhanvantry Hospital, Chandigarh, India
April 2011 – June 2011

Consultant Dentist - Dabur Dhanvantry Hospital, Chandigarh, India
July 2011 – July 2015

PROFESSIONAL SOCIETIES

National Student Research Group (NSRG)
August 2015 – Ongoing

Indian Dental Association (IDA)
January 2012 – Ongoing

PRESENTATIONS

Research!Louisville, Louisville, KY

October 2016

Poster Presentation: Mechanism of Interaction of Peptide Modified Nanoparticles with *Porphyromonas gingiva*.