Validation of an RPE-based submaximal oxygen consumption test using a total body recumbent stepper for individuals with spinal cord injury: a proof of concept study.

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VALIDATION OF AN RPE-BASED SUBMAXIMAL OXYGEN CONSUMPTION TEST USING A TOTAL BODY RECUMBENT STEPPER FOR INDIVIDUALS WITH SPINAL CORD INJURY: A PROOF OF CONCEPT STUDY

By

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A Thesis
Submitted to the Faculty of the College of Education and Human Development of the University of Louisville in Partial Fulfillment of the Requirements for the Degree of

Master of Science

Department of Exercise Physiology
University of Louisville
Louisville, Kentucky

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A Thesis Approved on

May 29, 2013

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Saori Hanaki-Martin, PhD.
DEDICATION

This thesis is dedicated to my parents

Mr. J. Stephen McCulloch

and

Mrs. Patricia J. McCulloch

who have always believed in me and have blessed me with so much.
ACKNOWLEDGEMENTS

I would like to thank my thesis advisor, Dr. Daniela Terson de Paleville, for her guidance, patience, and encouragement. I would also like to thank Dr. Ann Swank and Dr. Saori Hanaki-Martin for their comments and assistance. I wish to extend a huge thank you to Dr. Doug Lorenz for helping me with the statistics- without his help this would not have been possible. Finally, many thanks to my friends and family, without your support I would have been a mess.
ABSTRACT

VALIDATION OF AN RPE-BASED SUBMAXIMAL OXYGEN CONSUMPTION TEST USING A TOTAL BODY RECUMBENT STEPPER FOR INDIVIDUALS WITH SPINAL CORD INJURY: A PROOF OF CONCEPT STUDY

John P. McCulloch

May 29, 2013

Exercise training is crucial to improve cardiovascular health and quality of life in people with spinal cord injuries (SCI). A key limitation is the lack the validated tests to evaluate cardiovascular fitness in this population. The purpose of this study was to validate a submaximal test to predict maximal oxygen consumption in individuals with SCI. Ten able-bodied subjects and two individuals with SCI completed an RPE-based submaximal oxygen consumption test and a graded maximal oxygen consumption test on a NuStep T4 stepper. The results indicate that prediction of VO$_2$max from an RPE-based protocol is feasible and can produce reliable predicted VO$_2$max values in the able bodied population. This study is a proof of concept to the implementation of a submaximal test protocol using a total body recumbent stepper to predict VO$_2$max in able-bodied individuals. Additionally, this study shows evidence of feasibility of performing this test in SCI individuals.
# TABLE OF CONTENTS

DEDICATION .......................................................................................................................... iii

ACKNOWLEDGEMENTS ....................................................................................................... iv

ABSTRACT ............................................................................................................................. v

LIST OF FIGURES ................................................................................................................. vii

LIST OF TABLES ................................................................................................................ viii

INTRODUCTION .................................................................................................................. 1
  Cardiorespiratory Fitness ..................................................................................................... 1
  VO₂max Testing .................................................................................................................. 3
  Nervous System ................................................................................................................ 4
  Spinal Cord Injury ............................................................................................................. 8

METHODS ............................................................................................................................. 18
  Aims ................................................................................................................................... 18
  Hypothesis ........................................................................................................................ 18
  Experimental Design ......................................................................................................... 18
  Inclusion Criteria .............................................................................................................. 19
  VO₂peak Test Protocol ..................................................................................................... 20
  Submaximal Test Protocol ............................................................................................... 21
  Statistical Analysis ........................................................................................................... 21

RESULTS .............................................................................................................................. 23
  Subject Characteristics ..................................................................................................... 23
  Experimental Conditions ................................................................................................. 24
  Mixed Effects Model Building – Technical Considerations ............................................. 24
  Prediction Equations ......................................................................................................... 25
  RPE Only Model ............................................................................................................... 26
  Accuracy of Predicted VO₂ Max ...................................................................................... 27

CONCLUSION ....................................................................................................................... 30

REFERENCES ....................................................................................................................... 32

CURRICULUM VITAE ........................................................................................................... 39
LIST OF FIGURES

Figure 1: Organization of the nervous system ................................................................. 5
Figure 2: Cross-sectional view of the spinal cord. (VanPutte, Seeley, Regan, & Russo, 2011).... 7
Figure 3: International Standards Worksheet (page 1). (S. C. Kirshblum et al., 2011) ............ 11
Figure 4: International Standards Worksheet (page 2). (S. C. Kirshblum et al., 2011) .......... 11
Figure 5: Schematic illustration of the major organs and areas innervated by the sympathetic and parasympathetic nervous system according to spinal cord level. Taken from asiaresearchcenter.org. ................................................................. 13
Figure 6: Representative T1-weighted images from the upper thigh of (A) able-bodied (AB) female, (B) female with spinal cord injury (SCI) and low muscle fat, (C) male with SCI and high muscle fat, and (D) diabetic male with SCI and high intramuscular fat. (McCully et al., 2011) .... 14
Figure 7: Observed VO$_2$ from the submaximal exercise test (solid lines with dots) and maximal exercise test (dashed lines) tests. Marked X’s indicate VO$_2$ max predicted from the submaximal data.......................................................................................................................................................................................... 29
Figure 8: Observed vs. Predicted VO$_2$ max. Bars from points represent 95% confidence intervals of prediction. Observations for which confidence interval bars cross the dashed line are those for which the observed maximum VO$_2$ was contained in the 95% confidence. ........................................... 29
LIST OF TABLES

Table 1: Life expectancy for post injury by severity and age at injury. Taken from Spinal Cord Injury Facts and Figures at a Glance. (National Spinal Cord Injury Statistic Center, 2012)...........9
Table 2: Able Bodied Subject Characteristics ................................................................. 23
Table 3: SCI Subject Characteristics .................................................................................. 23
Table 4: VO₂, watts, and heart rate values recorded and correlating RPE during subject N89’s submaximal and maximal exercise tests ........................................................................... 24
Table 5: VO₂, and watt values recorded and correlating RPE during subject C28’s submaximal and maximal exercise tests ........................................................................... 24
Table 6: Estimates of fixed effects terms based on watts and RPE with 95% confidence intervals .......................................................................................................................................... 25
Table 7: Estimates of fixed effects based on RPE only with 95% confidence intervals .......... 26
Table 8: Observed and predicted VO₂ from RPE 9-17, 9-15, and 9-13 .................................. 28
INTRODUCTION

Cardiorespiratory Fitness

Cardiorespiratory fitness, which is a functional state of the respiratory, cardiovascular, and skeletal muscle systems, is necessary for an individual’s ability to perform moderate-to-high intensity exercise for prolonged periods of time (Caspersen, Powell, & Christenson, 1985; Pescatello, 2013). Low levels of cardiorespiratory fitness have been associated with an increased risk of premature death from all causes while an increase in cardiorespiratory fitness is associated with a decline in morbidity and mortality (Blair et al., 1995; Kodama et al., 2009; Paffenbarger Jr et al., 1993). High levels of cardiorespiratory fitness are associated with higher habitual levels of activity, and are associated with many health benefits (Haskell et al., 2007; Pate et al., 1995; Pescatello, 2013). Cardiovascular responses to physical activity depend on the type and intensity of the physical activity of the individual. Dynamic exercises that use large muscles groups will result in a larger response from the cardiovascular system than other types of exercise (Brooks, Fahey, & Baldwin, 2007).

Cardiorespiratory fitness of an individual is assessed by measuring their oxygen consumption (VO₂) levels at a maximal level of work (VO₂max) (Bruce, Kusumi, & Hosmer, 1973; Pescatello, 2013; Pollack, Schmidt, & Jackson, 1980; Shephard et al., 1968). The rate at which an individual consumes oxygen increases as the intensity of the activity increases. Higher VO₂max values indicate an individual is more fit, as their bodies are more efficient at consuming oxygen. The rate of oxygen transportation to
tissues, the capacity of the blood to carry oxygen, and the amount of oxygen taken from the blood all affect VO$_2$ and can be expressed in the following equation (Brooks et al., 2007):

$$\dot{V}O_2 = \dot{Q}(a - v)o_2$$

$\dot{Q}$ represents cardiac output, which is the amount of blood pumped by the left ventricle of the heart per minute. The two determinants of cardiac output are heart rate, which is the frequency of contractions of the heart per minute, and stroke volume, the amount of blood ejected from the heart during a single cardiac contraction. Cardiac output is expressed in liters/minute. Arteriovenous oxygen difference, expressed as $(a - v)o_2$, is the difference in oxygen content between the veins and arteries, essentially measuring how much oxygen was taken up by the tissues. This variable is expressed in milliliters of oxygen per 100 mL of blood or volumes percent (vol %) (Brooks et al., 2007).

Cardiac output and arteriovenous oxygen difference each account for about 50% of the increase in oxygen consumption during submaximal exercise (Brooks et al., 2007). As the intensity of exercise increases and approaches maximal levels, cardiac output plays an increasingly more important role in oxygen consumption, mainly due to an increasing heart rate. As the intensity of an exercise increases, oxygen uptake by active skeletal muscle also increases proportionally. This increase is mostly due to higher cardiac output. Endurance trained individuals show higher efficiency in both the uptake of oxygen by the tissues and cardiac output due to an increased stroke volume each time the heart contracts. Therefore, a more physically fit athlete will have a lower VO$_2$ at a
specific power output or intensity than an untrained individual exercising at the same power output or intensity (Brooks et al., 2007).

**VO₂max Testing**

Direct measurement of VO₂max is typically done using open circuit spirometry. In this procedure, an individual breathes through a low pressure valve that sends their expired air to a mixing chamber where the fractions of carbon dioxide, oxygen, and ventilation are analyzed by a pneumotachometer. Even with automated gas analysis, attention to detail during calibration is essential in order to obtain accurate results (Pescatello, 2013).

A maximal exercise test using open-circuit spirometry is considered to be the most accurate way to measure VO₂max since it directly measures the expired gas of a subject at a maximal workload (Noonan & Dean, 2000; Pescatello, 2013). However, maximal testing is not always possible or the best option for health professionals. Costs related to buying the equipment, paying technicians to run the equipment, and the space needed to run the test all restrict the ability to perform maximal tests to a mainly laboratory setting. Another issue with direct measurement maximal tests is that it requires the subject to exercise to volitional fatigue. This may require medical supervision and emergency equipment during the test. Often it is not worth the risk to put already at-risk subjects through a maximal test. Additionally, many patients do not want to exercise at high intensities. Measuring VO₂max with a maximal test, while accurate, may not be possible or safe for certain populations and situations.

For those situations when maximal testing is not possible or desirable, prediction of VO₂max through the use of submaximal tests is possible (Noonan & Dean, 2000;
Pescatello, 2013). A wide variety of submaximal tests have been validated by examining the relationship between directly measured VO\(_2\)max and predicted VO\(_2\)max from physiologic responses at a specific work rate or between directly measured VO\(_2\)max and test performance (Al-Rahamneh & Eston, 2011a, 2011b; Figoni, 2010; Hol, Eng, Miller, Sproule, & Krassioukov, 2007; Pescatello, 2013). The most common method of predicting VO\(_2\)max is with heart rate at specific workloads. While not as accurate in assessing an individual’s cardiovascular fitness, submaximal exercise tests are often preferred. Submaximal tests typically do not require expensive analysis equipment, they can be conducted outside of a laboratory setting, and are usually safer as the subject is not exercising to exhaustion.

*Nervous System*

The nervous system is a complex and vital network made up of the brain, spinal cord, nerves, and sensory receptors that coordinates the actions of all other body systems to maintain homeostasis with constantly changing stimuli (Cohen & Memmler, 2013; Wilmore, Costill, & Kenney, 2008). The nervous system maintains homeostasis in the body by constantly receiving sensory input both internally and externally, processing that information, and initiating and controlling a motor response (Cohen & Memmler, 2013; Jenkins, Kemnitz, & Tortora, 2007; Powers & Howley, 2009; Wilmore et al., 2008). The nervous system is composed of two parts: the central nervous system, made up of the brain and spinal cord, and peripheral nervous system, which includes all neurons outside the central nervous system (Cohen & Memmler, 2013; Jenkins et al., 2007; Powers & Howley, 2009; Wilmore et al., 2008).
The peripheral nervous system can be further divided according to function: the sensory (afferent) division, which sends sensory information to the central nervous system; and the motor (efferent) division, which carries out the actions dictated by the central nervous system (Powers & Howley, 2009; Wilmore et al., 2008). The motor division can then be further divided into the autonomic and somatic nervous systems (Cohen & Memmler, 2013; Jenkins et al., 2007; Powers & Howley, 2009; Wilmore et al., 2008). The somatic nervous system innervates skeletal muscle and can be voluntarily controlled (Cohen & Memmler, 2013; Jenkins et al., 2007; Powers & Howley, 2009; Wilmore et al., 2008). The autonomic nervous system innervates smooth muscle, cardiac muscle, and some glands (Cohen & Memmler, 2013; Jenkins et al., 2007; Powers & Howley, 2009). The heart, blood vessels, respiratory tract, and sweat glands are also under autonomic control (Jenkins et al., 2007; Krassioukov et al., 2012). The autonomic nervous system can be even further divided into sympathetic, parasympathetic, and enteric divisions (Jenkins et al., 2007; Wilmore et al., 2008). Effectors are typically innervated by both sympathetic and parasympathetic divisions and control opposing actions (Jenkins et al., 2007). The sympathetic division will prepare a body for activity while the parasympathetic division governs the body at rest (Jenkins et al., 2007).

Figure 1: Organization of the nervous system.
Sensory and motor impulses going to and from the brain must travel through the spinal cord (Cohen & Memmler, 2013; S. C. Kirshblum et al., 2011). Protected by the vertebrae, the spinal cord extends from the foramen magnum to the second lumbar vertebra and has four segments: cervical, thoracic, lumbar, and sacral (Cohen & Memmler, 2013; Jenkins et al., 2007). The spinal cord consists of gray matter, which is shaped like a butterfly, and white matter, which surrounds the gray matter. Gray matter is made up of the cell bodies of neurons, unmyelinated axons, dendrites, and neuroglia, receiving and integrating information coming to and from the spinal cord. White matter consists of myelinated axons and neurons and serves as the major pathway for the propagation of sensory and motor information to and from the brain, respectively (Jenkins et al., 2007; S. C. Kirshblum et al., 2011).

The gray matter is further subdivided into the anterior horns, posterior horns, and lateral horns (Jenkins et al., 2007). The cell bodies of somatic motor neurons are found in the anterior horns, providing nerve impulses for the skeletal muscles. The posterior horns receive input from sensory receptors, as they contain somatic and autonomic sensory neuron cell bodies. The lateral horns are only found in the thoracic, upper lumbar, and sacral segments of the spinal cord and contain cell bodies of autonomic motor neurons which regulate the activity of smooth muscle, cardiac muscle, and glands (Jenkins et al., 2007).

White matter is similarly divided into regions. The anterior and posterior horns of the gray matter divide the white matter into three columns: anterior, lateral, and posterior. These columns contain tracts that contain bundles of axons that either come from the same area, or are carrying similar information (Jenkins et al., 2007). Tracts that contain
axons bringing sensory information to the brain are called ascending tracts. The tracts carrying motor impulses down the spinal cord and away from the brain are called descending tracts (Jenkins et al., 2007).

Thirty-one pairs of spinal nerves branch from the spinal cord and are numbered according to the level at which they arise from the spinal cord (Cohen & Memmler, 2013). Two structures called roots attach each spinal nerve to the spinal cord. The dorsal root contains sensory axons, with the cell bodies of sensory neurons stored in the dorsal root ganglion (Cohen & Memmler, 2013; Jenkins et al., 2007). The ventral root is made up of motor neurons, with the cell bodies of these neurons stored in the anterior horns.

Figure 2: Cross-sectional view of the spinal cord. (VanPutte, Seeley, Regan, & Russo, 2011)
Each spinal nerve is named according to where it rises from the spinal cord (Cohen & Memmler, 2013; Jenkins et al., 2007). The nerves that arise from the inferior part of the spinal cord continue to travel down the vertebral column together until they each exit at a specific intervertebral foramen. This segment is called the cauda equina, meaning “horse’s tail” due to its similarity in appearance (Cohen & Memmler, 2013; Jenkins et al., 2007).

Spinal Cord Injury

Spinal cord injury (SCI) is a lesion of the spinal cord and affects the conduction of sensory and motor signals across the site of the lesion (Figoni, 2010; Waring et al., 2010). This leads to a variety of dysfunctions of motor, sensory, and autonomic control (Figoni, 2010; Theisen, 2012; West, Mills, & Krassioukov, 2012). It is estimated there are approximately 12,000 new SCI cases each year in the United States (National Spinal Cord Injury Statistic Center, 2012). The total number of people living with an SCI is estimated to be 265,000 individuals. SCI affects young adults more than any other age group, however the median age of incident has risen from 28.7 years old from 1973-1979 to 40.7 years of age in 2005 (National Spinal Cord Injury Statistic Center, 2012). Males are overwhelmingly more at risk than females, with 80.7% of spinal cord injuries reported to the national database. Motor vehicle accidents account for 40.4% of all spinal cord injuries, with the second most common being falls. The life expectancy of individuals with SCI has risen and will continue to increase, but they still have a shorter life expectancy than their able-bodied counterparts. The first year after the injury has a much higher mortality rate than during the subsequent years (National Spinal Cord Injury Statistic Center, 2012). Pneumonia and other respiratory illnesses are the most common
cause of death in the first year and thereafter (Brown, DiMarco, Hoit, & Garshick, 2006; Garshick et al., 2005). Reasons for a higher rate of mortality after SCI include level of lesion and completeness of injury, older age at injury, and injury in earlier calendar years (Brown et al., 2006; Garshick et al., 2005).

<table>
<thead>
<tr>
<th>Age at Injury</th>
<th>No SCI</th>
<th>Motor Functional at Any Level</th>
<th>Paralysis</th>
<th>Low Tetra (C5-C8)</th>
<th>High Tetra (C1-C4)</th>
<th>Ventilator Dependent at Any Level</th>
<th>Motor Functional at Any Level</th>
<th>Paralysis</th>
<th>Low Tetra (C5-C8)</th>
<th>High Tetra (C1-C4)</th>
<th>Ventilator Dependent at Any Level</th>
</tr>
</thead>
<tbody>
<tr>
<td>20</td>
<td>58.6</td>
<td>52.6</td>
<td>45.2</td>
<td>40.0</td>
<td>35.7</td>
<td>17.1</td>
<td>53.0</td>
<td>45.8</td>
<td>41.0</td>
<td>37.4</td>
<td>23.8</td>
</tr>
<tr>
<td>40</td>
<td>39.4</td>
<td>34.1</td>
<td>27.6</td>
<td>23.3</td>
<td>19.9</td>
<td>7.3</td>
<td>34.5</td>
<td>28.2</td>
<td>24.2</td>
<td>21.2</td>
<td>11.4</td>
</tr>
<tr>
<td>60</td>
<td>22.4</td>
<td>17.7</td>
<td>12.8</td>
<td>9.9</td>
<td>7.7</td>
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<td>18.0</td>
<td>13.2</td>
<td>10.4</td>
<td>8.6</td>
<td>3.2</td>
</tr>
</tbody>
</table>

Table 1: Life expectancy for post-injury by severity of injury and age at injury. Taken from Spinal Cord Injury Facts and Figures at a Glance. (National Spinal Cord Injury Statistic Center, 2012)

Lesion level and amount of damage to the spinal cord in the transverse plane play a large part in determining the consequences and severity of an SCI. The most obvious of these consequences is paralysis of the muscles that are innervated below the level of lesion. In complete spinal cord injuries, neuronal communication to and from the brain will be completely halted. Voluntary motor control below the lesion level may be lost, while a loss of inhibition from upper control centers may give rise to reflex contractions and muscle spasticity. Sensory information like muscle length, joint position, pain, temperature, and pressure may also be halted due to this interruption of the neural pathway. Testing the affected muscles and skin sensitivity can accurately determine the completeness of the injury as well as level of lesion (S. C. Kirshblum et al., 2011; Marino, 2007; Waring et al., 2010)

The International Standards for Neurological Classification of Spinal Cord Injury (ISNCSCI) with the ASIA Impairment Scale (AIS) is the most commonly used and accepted method for determining the severity and level of a lesion (S. C. Kirshblum et al.,
In this assessment, the patient undergoes a series of tests examining their sensory and motor function. The sensory test consists of light touch and pin pricks on both the left and right sides of the body for the different dermatomes. The motor preservation evaluation examines different myotomes (for example, elbow flexors are innervated by C5). Using the scores from the sensory and motor tests, the single neurological level of the injury can be determined by finding the most rostral of the sensory and motor levels.

The ASIA scale rates the severity on an A to E system (S. C. Kirshblum et al., 2011; Waring et al., 2010). A grade of “A” is considered “complete”; the patient has no sensory or motor function below the sacral segments S4-S5. “B” is called “sensory complete”, the patient has sensory function, but no motor function below the lesion level and includes the sacral segments S4-S5. “C” is “motor incomplete” where motor function is preserved below the neurological level, and more than half the muscles below the level of injury have a muscle grade below 3. “D” is also considered “motor incomplete”, however at least half of key muscle functions below the level of the lesion have a muscle grade equal to or greater than 3. “E” is considered “normal”, if a patient who has had prior deficits undergoes the INSCSCI testing and is graded normal, they receive this score. Non-SCI patients will not receive an AIS grade.
Figure 3: International Standards Worksheet (page 1). (S. C. Kirshblum et al., 2011)

Figure 4: International Standards Worksheet (page 2). (S. C. Kirshblum et al., 2011)
Spinal cord injuries are commonly separated into two groups based on the severity and level of injury. Impairment or loss of motor and/or sensory function in the thoracic, lumbar, or sacral segments of the spinal cord is referred to as paraplegia. Paraplegic subjects have arm function, but may have impaired function of the trunk, legs, and pelvic organs depending on the level of injury. Tetraplegia refers to impairment or loss of motor and/or sensory function in the cervical segments of the spinal cord. This may result in differing degrees of impairment of the four limbs as well as the trunk, legs, and pelvic organs (Chen et al., 2003; Marino, 2007; Waring et al., 2010). The most common type of SCI is incomplete tetraplegia (39.5%), followed by complete paraplegia (22.1%), incomplete paraplegia (21.7%), and complete tetraplegia (16.3%)(National Spinal Cord Injury Statistic Center, 2012).
Individuals with SCI are often physically unfit, and those with paraplegia are slightly more fit than those with tetraplegia (Eggers et al., 2001). The cross-sectional area of muscle fiber declines by 40-50% after injury. This change in muscle tissue may be associated with an increased risk of coronary artery disease (Figoni, 2010; Garshick et al., 2005; Nash & Dyson-Hudson, 2009; Phillips et al., 1998) and hyperlipidemia. There is also an increase in intramuscular fat, which may contribute to the onset of glucose intolerance and insulin dependence (Banerjea et al., 2008; McCully, Mulcahy, Ryan, & Zhao, 2011). Additional secondary complications include pulmonary emboli, pain, and reduced mobility (Walter et al., 2002). Individuals with chronic SCI have lower resting metabolic rates (RMR), resting energy expenditure (REE), and VO$_2$peak (Buchholz & Pencharz, 2004; Coutts, Rhodes, & McKenzie, 1983; Myers, Lee, & Kiratli, 2007; Phillips et al., 1998; Zurlo, Larson, Bogardus, & Ravussin, 1990).
Spinal cord injury may also impact autonomic function (Krassioukov, 2006, 2009; Krassioukov et al., 2012; Krassioukov & Claydon, 2006; Sisto et al., 2012; West et al., 2012). The cranial parasympathetic nervous system will not be affected and will remain intact. However, the sacral parasympathetic system may be affected by a complete SCI. Thoracolumbar sympathetic nervous system function can be affected to a varying degree, possibly disturbing heart function and blood redistribution capacity during exercise (Krassioukov, 2006, 2012; Sisto et al., 2012; Theisen, 2012). For this reason, heart rate may not be an accurate mean to predict VO₂max in the SCI population. The 6-20 RPE scale has shown a strong positive correlation with RPE, heart rate, and VO₂max in healthy populations (Al-Rahamneh & Eston, 2011a; Borg, 1982; Eston, Lamb, Parfitt, & King, 2005) and in individuals with SCI (Al-Rahamneh & Eston, 2011a, 2011b). Therefore, prediction of VO₂max based on RPE may be more reliable for the SCI population.
Spinal cord injury often reduces participation in physical activity (Buchholz, McGillivray, & Pencharz, 2003; Buchholz & Pencharz, 2004; Dallmeijer, Hopman, van As, & van der Woude, 1996; Fernhall, Heffernan, Jae, & Hedrick, 2008; Hoffman, 1986; Jacobs & Nash, 2004; Janssen, Dallmeijer, Veeger, & van der Woude, 2002; Lavis, Scelza, & Bockenek, 2007; Myers et al., 2007; Phillips et al., 1998) and decreases an individual’s resting metabolic rate (Buchholz et al., 2003; Buchholz & Pencharz, 2004; Hayes et al., 2005; McCully et al., 2011; Myers et al., 2007; Phillips et al., 1998; Price, 2010) which causes a major decrease in total daily energy expenditure. This decrease in total daily energy expenditure, combined with disorders of the autonomic nervous system commonly found in SCI patients (Garstang & Miller-Smith, 2007; Karlsson, 2006; Krassioukov, 2009; Krassioukov & Claydon, 2006; Teasell, Arnold, Krassioukov, & Delaney, 2000; Theisen, 2012; West et al., 2012), causes an increase in percent body fat (Buchholz & Pencharz, 2004; Flank, Wahman, Levi, & Fahlstrom, 2012; Gorgey et al., 2012), as well as places this population at a much higher risk of chronic diseases like cardiovascular disease (Cowan & Nash, 2010; Fernhall et al., 2008; Flank et al., 2012; Garshick et al., 2005; Myers et al., 2007; Svircev, 2009), obesity (Buchholz et al., 2003; Buchholz & Pencharz, 2004; Fernhall et al., 2008; Flank et al., 2012; Garshick et al., 2005; Gater, 2007), and diabetes (Banerjea et al., 2008; Flank et al., 2012; Garshick et al., 2005).

Many chronic diseases such as type 2 diabetes, cardiovascular disease, and obesity are associated with lifestyle behaviors like maintaining a positive energy balance. This positive energy balance in otherwise healthy populations is caused by a sedentary lifestyle, increased caloric intake, a reduction in metabolism, or a mixture of these
factors. Total daily energy expenditure and physical activity is inversely related to weight gain and body fat percentage. As an individual’s daily energy expenditure decreases, over time their weight and percent body fat will increase due to the positive energy balance they maintain (Ravussin et al., 1988).

Exercise training individuals with spinal cord injury has shown positive results in relation to cardiovascular health and overall quality of life (Cowan & Nash, 2010; Dobkin et al., 2007; Gorgey et al., 2012; Hettinga & Andrews, 2008; Hicks et al., 2005; Hicks et al., 2003; Hoffman, 1986; Jacobs, Nash, & Rusinowski, 2001; S. Kirshblum, 2004; Le Foll-de Moro, Tordi, Lonsdorfer, & Lonsdorfer, 2005; L. Valent et al., 2010; L. Valent, Dallmeijer, Houdijk, Talsma, & van der Woude, 2007; L. J. Valent et al., 2009; van Duijnhoven et al., 2010). The most accurate measurement of cardiovascular fitness in healthy individuals is through the measurement of oxygen consumption at an individual’s maximal work rate (VO$_2$max). VO$_2$max is commonly used for exercise prescription as it gives the health professional an objective measurement of the cardiovascular fitness of an individual (Bruce et al., 1973; Noonan & Dean, 2000; Pescatello, 2013; Pollack et al., 1980; Shephard et al., 1968). However, maximal effort tests cannot be done without the use of expensive equipment typically only found in labs, are time consuming, and cannot be conducted without a doctor’s consent.

Tests estimating VO$_2$max from submaximal levels of work are much affordable, do not require the patients to exercise to exhaustion, are typically safer, and are commonly used to estimate the maximal oxygen consumption of healthy populations (Noonan & Dean, 2000; Pescatello, 2013). Most studies that have developed a submaximal exercise protocol for the SCI population have depended on stressing the
cardiovascular system with only the upper body (Al-Rahamneh & Eston, 2011a, 2011b; Borello-France et al., 2000; Hol et al., 2007; van Drongelen, Maas, Scheel-Sailer, & Van Der Woude, 2009; Verellen, Meyer, Janssens, & Vanlandewijck, 2012). However, the small and easily exhaustible muscles of the upper body often do not adequately stress the cardiovascular system, resulting in lower oxygen consumption values (Coutts et al., 1983; Eggers et al., 2001).

In a study comparing cardiovascular responses between able bodied individuals and individuals with spinal cord injury, Higuchi et al. (2006) found that passive walking resulted in similar values for oxygen consumption, pulmonary ventilation, and heart rate in individuals with SCI when compared to able bodied subjects. Therefore, even passive use of the muscles of the lower body may increase an individual with spinal cord injury’s cardiovascular response to exercise. A total body recumbent stepper may be a feasible option that could potentially elicit the same cardiovascular responses to exercise as passive walking. Maximal tests using a total body recumbent stepper have been established for both able bodied individuals (Billinger, Loudon, & Gajewski, 2008) and individuals with stroke (Billinger, Tseng, & Kluding, 2008).

Al-Rahamneh and Eston (2011a) reported that a submaximal exercise protocol using an arm crank ergometer to estimate maximal oxygen consumption in individuals with SCI show high correlation with the directly measured values from a maximal test. Since RPE may be a more reliable indicator of cardiovascular stress in individuals with spinal cord injury than heart rate, the current study will attempt to establish a submaximal protocol based off of RPE using a total body recumbent stepper.
METHODS

Aims
The purpose of this study is to validate a submaximal test to predict maximal oxygen consumption using RPE in individuals with spinal cord injury.

Hypothesis
1. Values of VO₂ max estimated by a submaximal test in a total body recumbent stepper will show a strong positive correlation with the values of VO₂peak obtained from a maximal graded exercise test.

Experimental Design
Participants with and without spinal cord injuries were invited to participate in this study. The study took place at The Frazier Rehab Institute. Each participant performed a graded exercise test (GXT) on a total body recumbent stepper (NuStep T4 ergometer, Ann Arbor, MI) to measure peak oxygen consumption (VO₂peak) and a submaximal test to estimate VO₂max. The tests were separated by at least 48 hours and at most one week. The submaximal test was conducted first to avoid familiarization with the full RPE scale. Participants were asked to not perform any moderate or heavy exercise 12 hours prior to the test. Each test was conducted on the same total body recumbent stepper. The seat position was set so the subject had a slight bend in their knee at full extension. Arm handles were positioned to allow full extension without leaning forward in the seat.
Oxygen consumption was analyzed with a Parvo Medic TrueOne 2400 (Sandy, UT). Analysis of the expired air occurred every 10 seconds. The cart was calibrated with a 3-liter syringe for flowmeter calibration and the ambient air measure for gas calibration at least 30 minutes before testing as recommended by the manufacturer’s guidelines. Heart rate was recorded using a Polar heart rate monitor as well as by 3-lead EKG. RPE was recorded using the Borg 6-20 scale, which was explained to each participant using standardized instructions. Any questions the participant had were answered to insure full understanding. All variables such as gas consumption, respiratory exchange ratio, heart rate, $V_E$, power output, and time were all kept out of the participant’s sight during the test.

**Inclusion Criteria**

Able bodied individuals and individuals with chronic spinal cord injury (SCI) aged 18-65 in stable medical condition without cardiopulmonary disease were invited to participate in this study. Individuals with SCI that met the following inclusion criteria were included in the study:

- Have no:
  - Painful musculoskeletal dysfunction.
  - Unhealed fracture, contracture, pressure sore.
  - Urinary tract infection.
  - Clinically significant depression.
  - Psychiatric disorders.
  - Ongoing drug abuse.
• Clear indications that the period of spinal shock is concluded which will be determined by the presence of muscle tone, deep tendon reflexes, and muscle spasms.

• Participants must have non-progressive SCI with injuries between spinal segments Cervical 2 to Sacral 5 and an American Spinal Injury Association Impairment Scale (AIS) classification of A-D.

• Participants must not be ventilator dependent for respiration.

• Participants will be excluded if there is a presence of:
  o major cardiovascular or pulmonary disease
  o pregnancy
  o endocrine disorders
  o malignancy
  o marked obesity
  o lower extremity deep vein thrombosis
  o Major gastrointestinal problems such as swallowing, or other major medical illness contraindicated for a maximal and submaximal exercise test, spirometry, or oxygen consumption test.

Prior to the study, potential participants will be evaluated by a physician, Dr. Williams, who will recommend or contraindicate participation.

**VO₂peak Test Protocol**

Participants warmed up for two minutes at a resistance of 1 and at 115 steps per minute (SPM) for able bodied subjects and 80 SPM for SCI subjects as these speeds have been validated (Billinger, Loudon, et al., 2008; Billinger, Tseng, et al., 2008). After the
two minute warm up, the subjects immediately began the test at a resistance of 4. Every two minutes, the resistance was increased until exhaustion. 20 seconds before the end of each stage, the subjects were asked to report their RPE. Blood pressure and heart rate were measured before warm up, immediately after the test, and 5 minutes posttest. The test was terminated when 1) the subject reports subjective fatigue and stops the test despite verbal encouragement, 2) the subject is no longer able to keep the SPM at or above 115 for able bodied subjects and 80 for SCI subjects, and 3) predicted maximum heart rate was reached.

**Submaximal Test Protocol**

Participants warmed up for two minutes at a resistance of 1 and at 115 SPM for able bodied subjects and 80 SPM for SCI subjects. The subjects were then asked to complete 5 two minute stages at RPEs of 9, 11, 13, 15, and 17. Every 30 seconds subjects were asked their RPE. If their RPE was anything other than the RPE assigned for that stage, resistance was adjusted. Watts and heart rate were all also taken every 30 seconds. Blood pressure and heart rate were measured before warm up, immediately after the test, and 5 minutes posttest. Subjects were instructed to cool down at a resistance of 1 and at their own pace for two minutes after blood pressure and heart rate were taken immediately posttest.

**Statistical Analysis**

Linear mixed effects models were fit using data from the submaximal test. The fixed effects were defined so that submaximal VO2 was modeled as a linear function of RPE and average wattage during the submaximal test. Random effects were defined for
the intercept and RPE slope term. Estimates of the intercept and slope terms with 95% confidence intervals were generated from the mixed effects model.

Predictions of maximum VO$_2$ were generated from these models using the fixed effects equation and the best linear unbiased predictors (BLUP) of the random effects. For these predictions, we set RPE = 20 to correspond with the maximal test. Since the submaximal test terminates at RPE = 17, average wattage at RPE = 20 was not known and could not be used to predict maximum VO$_2$ at an RPE of 20. A mixed effects model of average wattage onto RPE was fit to generate predicted average wattages at RPE 20. These predicted wattage values were subsequently used to generate predicted maximum VO$_2$ values for each individual. As a secondary measure, we fit mixed effects models excluding the wattage term, and generated predicted maximum VO$_2$ at RPE = 20 from these models. Pearson correlation coefficients and Lin’s concordance correlation coefficient were calculated between observed and predicted VO$_2$.

In an effort to determine the extent to which the submaximal test must be conducted, (i.e.) at what RPE the submaximal test can be terminated, models were fit for all of the submaximal test data (RPE 9 – 17), a subset of the data including only RPE 9 – 15, and another subset including only RPE 9 – 13. Predictions from each of these models were generated as described above, and the Pearson and Lin correlations between predicted and observed maximum VO$_2$ was calculated.
RESULTS

Subject Characteristics

**Table 2: Able Bodied Subject Characteristics**

<table>
<thead>
<tr>
<th>Subject</th>
<th>Age</th>
<th>Sex</th>
<th>Weight (kg)</th>
<th>Height (cm)</th>
<th>Maximum Reported RPE</th>
<th>RER</th>
<th>HR</th>
<th>Watts</th>
<th>Resistance</th>
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<tbody>
<tr>
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<td>F</td>
<td>67.1</td>
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<td>M</td>
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<td>174.6</td>
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<td>1.21</td>
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<td>F</td>
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<td>1.07</td>
<td>176.0</td>
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**Summary Mean (SD)**

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<tr>
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<td>29 (5.72)</td>
<td>28 (5.62)</td>
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<td>4</td>
<td>10</td>
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<td>Weight (kg)</td>
<td>69.83 (13.89)</td>
<td>66.38 (0.85)</td>
<td>69.1 (5.1)</td>
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<tr>
<td>Height (cm)</td>
<td>177.8 (4.53)</td>
<td>168.13 (7.96)</td>
<td>179.1 (1.8)</td>
</tr>
<tr>
<td>Maximum Reported RPE</td>
<td>19.5 (0.55)</td>
<td>19.4 (0.70)</td>
<td>19.4 (0.70)</td>
</tr>
<tr>
<td>RER</td>
<td>1.15 (0.06)</td>
<td>1.17 (0.08)</td>
<td>1.17 (0.08)</td>
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<td>HR</td>
<td>178.25 (10.19)</td>
<td>183.33 (9.42)</td>
<td>180.28 (9.70)</td>
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<tr>
<td>Watts</td>
<td>287.42 (48.97)</td>
<td>180.13 (35.75)</td>
<td>244.5 (69.48)</td>
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<td>Resistance</td>
<td>9 (0.89)</td>
<td>8 (0.82)</td>
<td>8.6 (0.97)</td>
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**Table 3: SCI Subject Characteristics**

Six male and five female able bodied subjects initially participated in the submaximal and maximal oxygen consumption tests. However, one female subject was not able to complete the two tests within seven days of each other and was training for a marathon. Therefore, her data was excluded from analysis due to her training increasing her recorded oxygen consumption during the maximal test. The average age of the ten remaining participants was 28 with a standard deviation of 5.62. The ages ranged from 20 years to 37 years old. The average RPE recorded at the end of the maximal test was 19.4 (SD: 0.70) with the lowest being 18. Average respiratory exchange ratio at peak RPE was 1.17 (0.08). Average heart rate was 180.28 (9.70) beats per minute. Average wattage of the participants at maximum RPE was 244.5 W (69.48) with a maximum of 382.5 W.
(Subject 2) and a minimum of 147 W (Subject 1). Two males with thoracic spinal cord injuries also participated in the submaximal and maximal oxygen consumption tests. Both reported a maximum RPE of 20 during the maximal test. Their average wattage at maximal RPE was 118.5 and the average RER was 1.17.

**Experimental Conditions**

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<tr>
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<tr>
<td><strong>Submax Watts</strong></td>
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<td>87.8</td>
<td>112.5</td>
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<td><strong>Submax HR</strong></td>
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<td>Maximal HR</td>
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</table>

Table 4: VO₂, watts, and heart rate values recorded and correlating RPE during subject N89’s submaximal and maximal exercise tests

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<th>17</th>
<th>18</th>
<th>19</th>
<th>20</th>
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<tbody>
<tr>
<td><strong>Submax VO₂</strong></td>
<td>11.9</td>
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</tr>
<tr>
<td>Maximal VO₂</td>
<td>12.2</td>
<td>12.5</td>
<td>15.3</td>
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</tr>
<tr>
<td><strong>Submax Watts</strong></td>
<td>62.8</td>
<td>85.0</td>
<td>70.5</td>
<td>94.0</td>
<td></td>
<td></td>
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</tr>
<tr>
<td>Maximal Watts</td>
<td>60.0</td>
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</tbody>
</table>

Table 5: VO₂, and watt values recorded and correlating RPE during subject C28’s submaximal and maximal exercise tests

The two tables above are the results of four tests from two participants, one able bodied and the other with an SCI. Wattage was recorded four times during the submaximal test and two times during the maximal test. The listed VO₂ is the average of the three highest oxygen consumption values during each stage. The SCI subject was only able to make it 30 seconds into his last stage before exhaustion, only giving two VO₂ values.

**Mixed Effects Model Building – Technical Considerations**

The mixed effects models of the submaximal data were built progressively. The initial linear model of VO₂ included RPE as the lone fixed effect and only random a intercept term. Adding a random RPE slope term significantly improved the fit of the model (ANOVA, p < .001), and thus the random RPE slope term was included. The
average wattage fixed effect was significant when added to the random RPE model (p < .001) and was therefore included. A random wattage term did not significantly improve the fit of the model (ANOVA, p > .13) and was thus excluded. These findings defined the mixed effects model specification detailed in the methods section, and were consistent for each of the ranges of RPE tested (RPE 9-17, RPE 9-15, and RPE 9-13).

**Prediction Equations**

Estimates of the fixed effects terms (intercept, RPE slope, wattage slope) with 95% confidence intervals are in the table below. Predictably, VO2 increased with RPE and wattage, although the rate at which VO2 increased with RPE varied substantially based on the subset of the data used, from 0.503 per RPE unit for the full data to 0.631 per RPE unit for the 9-15 RPE subset of the data. The rate at which VO2 increased with average wattage was observed to be lower for the subsets of the data (0.099 and 0.099) than for the full data (0.112).

<table>
<thead>
<tr>
<th>Data</th>
<th>Intercept</th>
<th>RPE Slope</th>
<th>Wattage Slope</th>
</tr>
</thead>
<tbody>
<tr>
<td>RPE 9-17</td>
<td>-1.990 (-3.694, -0.287)</td>
<td>0.503 (0.200, 0.805)</td>
<td>0.112 (0.094, 0.29)</td>
</tr>
<tr>
<td>RPE 9-15</td>
<td>-1.854 (-3.866, 0.157)</td>
<td>0.631 (0.314, 0.948)</td>
<td>0.099 (0.079, 0.118)</td>
</tr>
<tr>
<td>RPE 9-13</td>
<td>-0.613 (-3.573, 2.348)</td>
<td>0.521 (0.179, 0.862)</td>
<td>0.098 (0.076, 0.120)</td>
</tr>
</tbody>
</table>

_Table 6: Estimates of fixed effects terms based on watts and RPE with 95% confidence intervals_

The fixed effects equations defining VO2 as a linear function of RPE and wattage were defined based on the fixed effects estimates in the above table:

- **RPE 9-17:** $VO_2 = -1.990 + 0.503 \times RPE + 0.112 \times Watts$
- **RPE 9-15:** $VO_2 = -1.854 + 0.631 \times RPE + 0.099 \times Watts$
- **RPE 9-13:** $VO_2 = -0.613 + 0.521 \times RPE + 0.098 \times Watts$
It should be noted that these equations provide population-level predictions rather than individualized predictions afforded by the random effects included in the model. Specifically, the predicted maximum VO$_2$ was generated using the above fixed intercepts and slopes as well as the BLUP of the random effects, (i.e.) the individual-level deviations from the intercept and RPE-slope terms. Because of this, these equations are not meant for general use in predicting maximum VO$_2$ based on RPE and average wattage. Correlations between the population predictions of maximum VO$_2$ based on the above equations and the observed maximum VO$_2$ were much lower than those for the predictions that utilized the random effects detailed in the next section.

*RPE Only Model*

Average wattage was a significant predictor in the VO$_2$ models of the submaximal test data, but pose a challenge in predicting maximum VO$_2$, since the average wattage at RPE = 20 is unknown and must itself be predicted. Further, although average wattage was a significant predictor of VO$_2$ for the submaximal data, it was not known if it contributed substantially to prediction of the observed maximum VO$_2$. Therefore, mixed effects models without the average wattage fixed effect were fit. Estimates of the fixed effects for the intercept and RPE slope with 95% confidence intervals are provided below.

<table>
<thead>
<tr>
<th>Data</th>
<th>Intercept</th>
<th>RPE Slope</th>
</tr>
</thead>
<tbody>
<tr>
<td>Full data (RPE 9-17)</td>
<td>-4.986</td>
<td>1.998</td>
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<tr>
<td></td>
<td>(-9.251, -0.721)</td>
<td>(1.574, 2.422)</td>
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<tr>
<td>Sub data 1 (RPE 9-15)</td>
<td>-3.919</td>
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<td>(-8.046, 0.208)</td>
<td>(1.456, 2.346)</td>
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<tr>
<td>Sub data 2 (RPE 9-13)</td>
<td>-0.624</td>
<td>1.582</td>
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<tr>
<td></td>
<td>(-4.805, 3.557)</td>
<td>(1.129, 2.035)</td>
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</tbody>
</table>

*Table 7: Estimates of fixed effects based on RPE only with 95% confidence intervals*
Fixed effects equations for predicting VO$_2$ from the RPE-Only models are below. As before, the actual predictions include the BLUP of the random effects (deviations from the intercept and slope, per patient) and are only partially generated from these equations.

- **RPE 9-17:** \( \text{VO}_2 = -4.986 + 1.998 \times \text{RPE} \)
- **RPE 9-15:** \( \text{VO}_2 = -3.919 + 1.901 \times \text{RPE} \)
- **RPE 9-13:** \( \text{VO}_2 = -0.624 + 1.582 \times \text{RPE} \)

**Accuracy of Predicted VO$_2$ Max**

The table below lists the observed maximum VO$_2$ and maximum VO$_2$ predicted from each subset of the data with each VO$_2$ model. Correlation and concordance coefficients and 95% confidence intervals are provided for each of the predictions. Predictions offered by the full data (RPE 9-17) correlated well with observed values. Correlations for the RPE + Watts and RPE-Only model exceeded 0.86 and concordance correlations exceeded 0.81. Substantial accuracy was lost in using only RPE 9-15 and RPE 9-13 in prediction, as correlation coefficients were reduced from the correlations exhibited for the RPE 9-17 predictions. It was noteworthy that the correlation exhibited by the RPE-Only predictions \( (r = 0.86) \) was only slightly and non-significantly \( (p = .89) \) lower than the correlation exhibited by the RPE + Watts predictions \( (r = 0.88) \).
Table 8: Observed and predicted VO$_2$ from RPE 9-17, 9-15, and 9-13

The residual standard error for predicting maximum VO$_2$ from the RPE-Only, 9-17 mixed effects model was 2.09, indicating that 95% confidence intervals for prediction would vary approximately 4.09 in either direction from the prediction. Six of the 10 confidence intervals for predicted maximum VO$_2$ contained the observed maximum VO$_2$ in our sample. Further, six of the 10 predicted maximum VO$_2$ were within 10% of the observed values. Residual standard errors and confidence interval coverage rates were not calculated for other models – the RPE-Only model did not significantly differ in predictive accuracy from the RPE + Watts model and models using subsets of the data (RPE 9-15 and 9-13) were not sufficiently accurate in predicting maximum VO$_2$. 

<table>
<thead>
<tr>
<th>Subject</th>
<th>Observed</th>
<th>RPE 9-17</th>
<th>RPE 9-15</th>
<th>RPE 9-13</th>
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<tr>
<td></td>
<td></td>
<td>RPE + Watts</td>
<td>RPE-Only</td>
<td>RPE + Watts</td>
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<td>N69</td>
<td>38.1</td>
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<td>35.6</td>
<td>32.8</td>
</tr>
<tr>
<td>Mean (SD)</td>
<td>33.4 (5.9)</td>
<td>34.5 (7.6)</td>
<td>35.0 (7.5)</td>
<td>34.1 (8.1)</td>
</tr>
</tbody>
</table>

Correlation

<table>
<thead>
<tr>
<th>Correlation</th>
<th>RPE 9-17</th>
<th>RPE 9-15</th>
<th>RPE 9-13</th>
</tr>
</thead>
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<tr>
<td></td>
<td>0.88</td>
<td>0.71</td>
<td>0.30</td>
</tr>
<tr>
<td></td>
<td>(0.57, 0.97)</td>
<td>(0.14, 0.92)</td>
<td>(-0.41, 0.78)</td>
</tr>
<tr>
<td></td>
<td>0.86</td>
<td>0.65</td>
<td>0.33</td>
</tr>
<tr>
<td></td>
<td>(0.49, 0.97)</td>
<td>(0.04, 0.91)</td>
<td>(-0.37, 0.80)</td>
</tr>
</tbody>
</table>

Concordance

<table>
<thead>
<tr>
<th>Concordance</th>
<th>RPE 9-17</th>
<th>RPE 9-15</th>
<th>RPE 9-13</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>0.83</td>
<td>0.67</td>
<td>0.27</td>
</tr>
<tr>
<td></td>
<td>(0.53, 0.95)</td>
<td>(0.08, 0.88)</td>
<td>(-0.34, 0.72)</td>
</tr>
<tr>
<td></td>
<td>0.81</td>
<td>0.63</td>
<td>0.30</td>
</tr>
<tr>
<td></td>
<td>(0.47, 0.94)</td>
<td>(0.08, 0.88)</td>
<td>(-0.31, 0.74)</td>
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</tbody>
</table>
Figure 7: Observed VO$_2$ from the submaximal exercise test (solid lines with dots) and maximal exercise test (dashed lines) tests. Marked X’s indicate VO$_2$ max predicted from the submaximal data.

Figure 8: Observed vs. Predicted VO$_2$ max. Bars from points represent 95% confidence intervals of prediction. Observations for which confidence interval bars cross the dashed line are those for which the observed maximum VO$_2$ was contained in the 95% confidence.
CONCLUSION

The results indicate that prediction of VO$_2$max from an RPE-based protocol is feasible and can produce reliable predicted VO$_2$max values in the able bodied population. This is in agreement with previous studies on RPE and VO$_2$max prediction (Al-Rahamneh & Eston, 2011a, 2011b; Eston et al., 2005). However, unlike what Al-Rahamneh and Eston (2011a) found, ending the test at RPE 13 or RPE 15 results in a significant loss of accuracy in predicting VO$_2$max. As a result, future tests must run until RPE 17 with further examination of ending the tests at lower RPEs.

Also note that the regression equations developed in this study are based solely on the 10 able bodied subjects tested and are not intended for widespread use in either SCI or able bodied populations. If a healthcare professional wished to use this protocol, they should plot that specific subject’s VO$_2$ and RPE values and develop their own linear regression equation to predict VO$_2$max by extrapolating out to RPE 20. The prediction equations accounting for watts did give values that were better correlated to the directly measured values than the equations based solely on RPE. However, the small increase in correlation (.88 vs. .86) was not statistically significant. The inclusion of watts in future prediction equations should be considered optional. In fact, including watts may result in an additional source of error in the predicted values since an estimation of watts at RPE 20 would also be necessary.

This study is a proof of concept of the feasibility to use a submaximal test protocol using a total body recumbent stepper to predict VO$_2$max in able bodied
individuals. Additionally, this study shows evidence of feasibility in one individual with motor complete and one subject with motor incomplete SCI. Future directions include creating prediction equations for a larger group of individuals with different levels and severity of SCI.
REFERENCES


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Thesis: VALIDATION OF AN RPE-BASED SUBMAXIMAL OXYGEN CONSUMPTION TEST USING A TOTAL BODY RECUMBENT STEPPER FOR INDIVIDUALS WITH SPINAL CORD INJURY: A PROOF OF CONCEPT STUDY

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**Studies**

1. **John McCulloch, B.S.**; Ann Swank, Ph.D.; Sevda Aslan, Ph.D.; Saori Hanaki-Martin, Ph.D.; Douglas Lorenz, Ph.D.; Daniela Terson de Paleville, Ph.D.
   VALIDATION OF AN RPE-BASED SUBMAXIMAL OXYGEN CONSUMPTION TEST USING A TOTAL BODY RECUMBENT STEPPER FOR INDIVIDUALS WITH SPINAL CORD INJURY: A PROOF OF CONCEPT STUDY. 2013.

   Effect of Resistance Training and Aerobic Conditioning on Muscular Strength and Submaximal Fitness for Individuals with Chronic Heart Failure: Influence of Type 2 Diabetes. 2012.

   Effect of Topical Menthol on Aerobic Capacity. 2012.

**Conferences**


2. Research!Louisville, Louisville, KY, 2012. Effect of Resistance Training and Aerobic Conditioning on Muscular Strength and Submaximal Fitness for Individuals with Chronic Heart Failure: Influence of Type 2 Diabetes.

3. Experimental Biology, Boston, MA, 2013. Validation of submaximal oxygen consumption tests using an arm crank ergometer and NuStep ergometer for individuals with spinal cord injury. *(Abstract submitted)*
Certifications and Memberships

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- American Heart Association First Aid (Expires May 2013)
- Member of the National Strength and Conditioning Association (2010 - Present)
- Member of the American College of Sports Medicine (2012 - Present)

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  - Teach health and fitness courses
  - Assist in teaching undergraduate courses
  - Run physical fitness assessment tests
  - Assist with ongoing studies

University of Dayton Rec Plex, Dayton, OH
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Fitness Attendant
  - Supervise facility
  - Run fitness assessments
  - Clean and fix equipment
  - Act as first responder in case of emergency

Other Experience

Minnesota Sport and Spine Rehabilitation, Burnsville, MN
May 2009-August 2009
Student Intern
  - Observed assessment and treatment of sport, work, and general injuries

Capernaum Pediatrics, New Hope, MN
June 2009-August 2009
Student Intern
  - Observed treatment of children with various mental disabilities ranging from severe downs-syndrome to mild cerebral palsy

Methodist Hospital, St. Louis Park, MN
June 2002-May 2005
Volunteer
  - Discharged patients, ran errands for doctors and nurses, delivered medications to nursing stations
Activities, Honors, and Awards

- University of Louisville Graduate School Dean’s Citation Award Winner 2013
- University of Louisville Exercise Physiology Outstanding Student Award 2013
- University of Louisville Health and Human Performance Club
  - Club Founder: formed January 2012
  - President: January 2012 – Present
- President’s Scholarship at the University of Dayton for holding GPA over 3.0
- Pre-Physical Therapy Club: September 2008-2011
- University of Dayton Men’s Crew team 2007-2010
  - Fundraising Chair: November 2008-December 2009
  - Treasurer: January 2009-June 2009
- Eagle Scout awarded December 2006